



# DECLARATION OF CONFLICT OF INTEREST OR RELATIONSHIP

Speaker Name: Terry Oakes

I have no conflicts of interest to disclose with regard to the subject matter of this presentation.

*Toronto!*

# Artifacts in fMRI



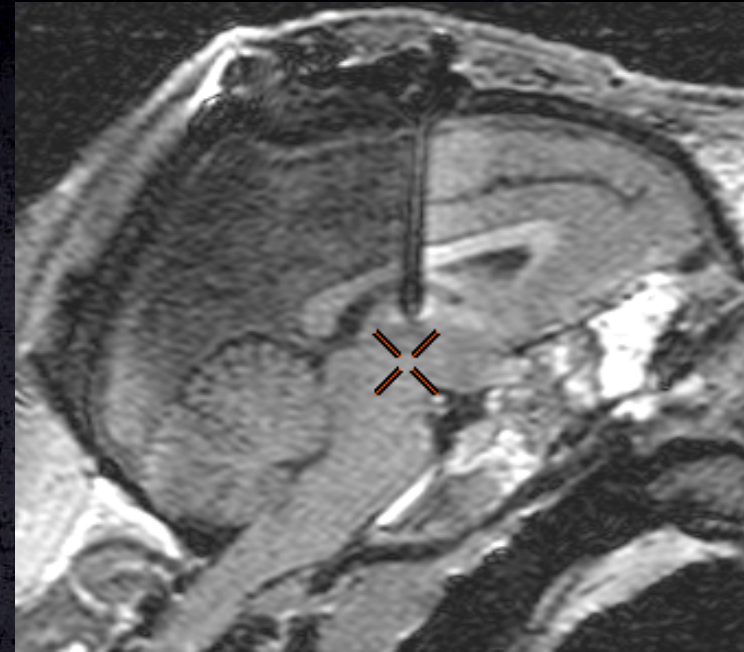
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THE UNIVERSITY  
of  
**WISCONSIN**  
MADISON

What I can tell you about:

- PET imaging
- Radionuclide production
- PET data analysis
- fMRI data analysis
- Coregistration
- Morphometry measures

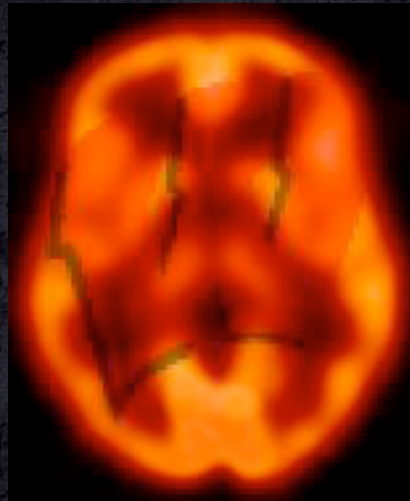


Not so much:

MRI physics, pulse sequences, data acquisition

# What is an Artifact?

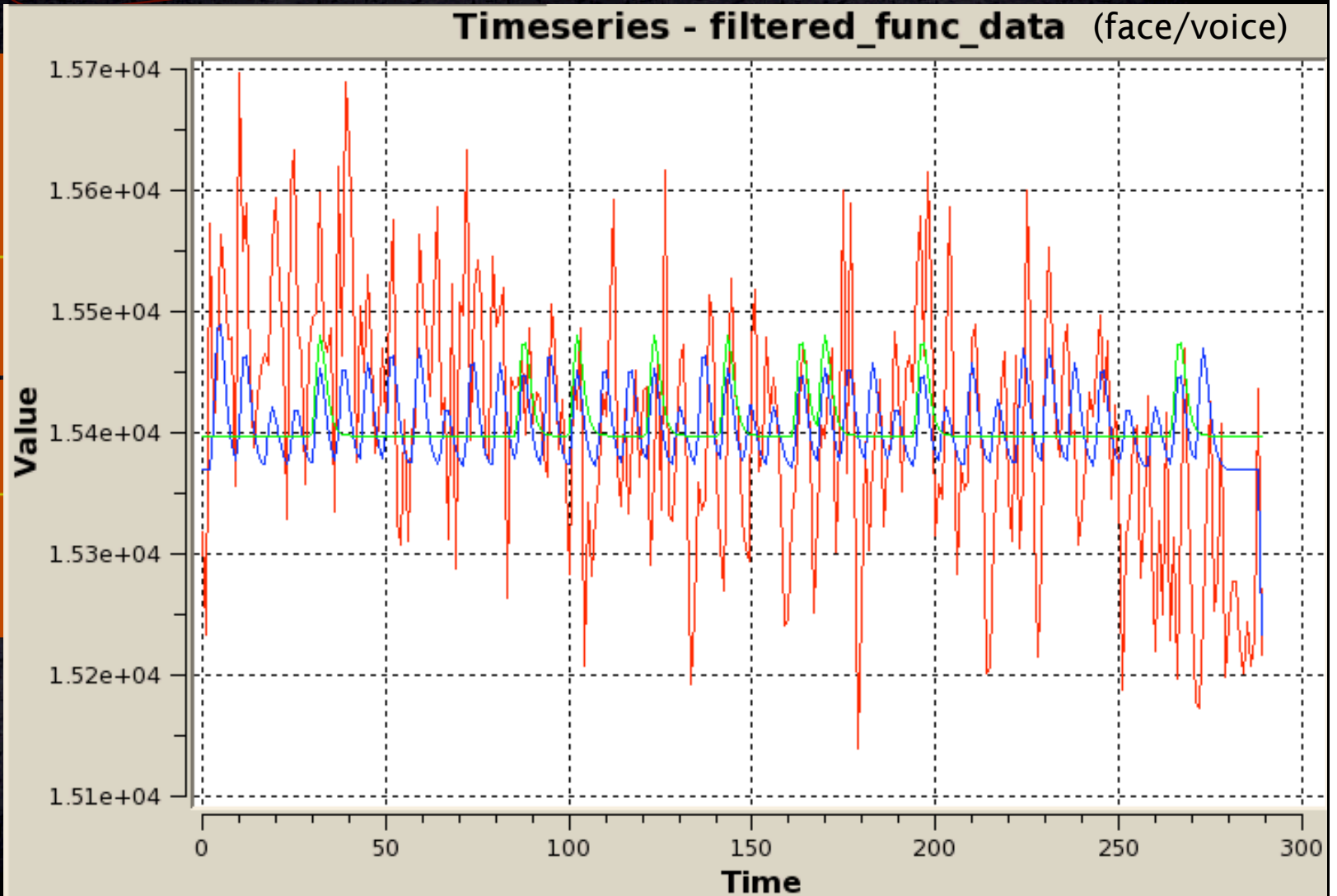
To neuroscientists, this brain looks funny.



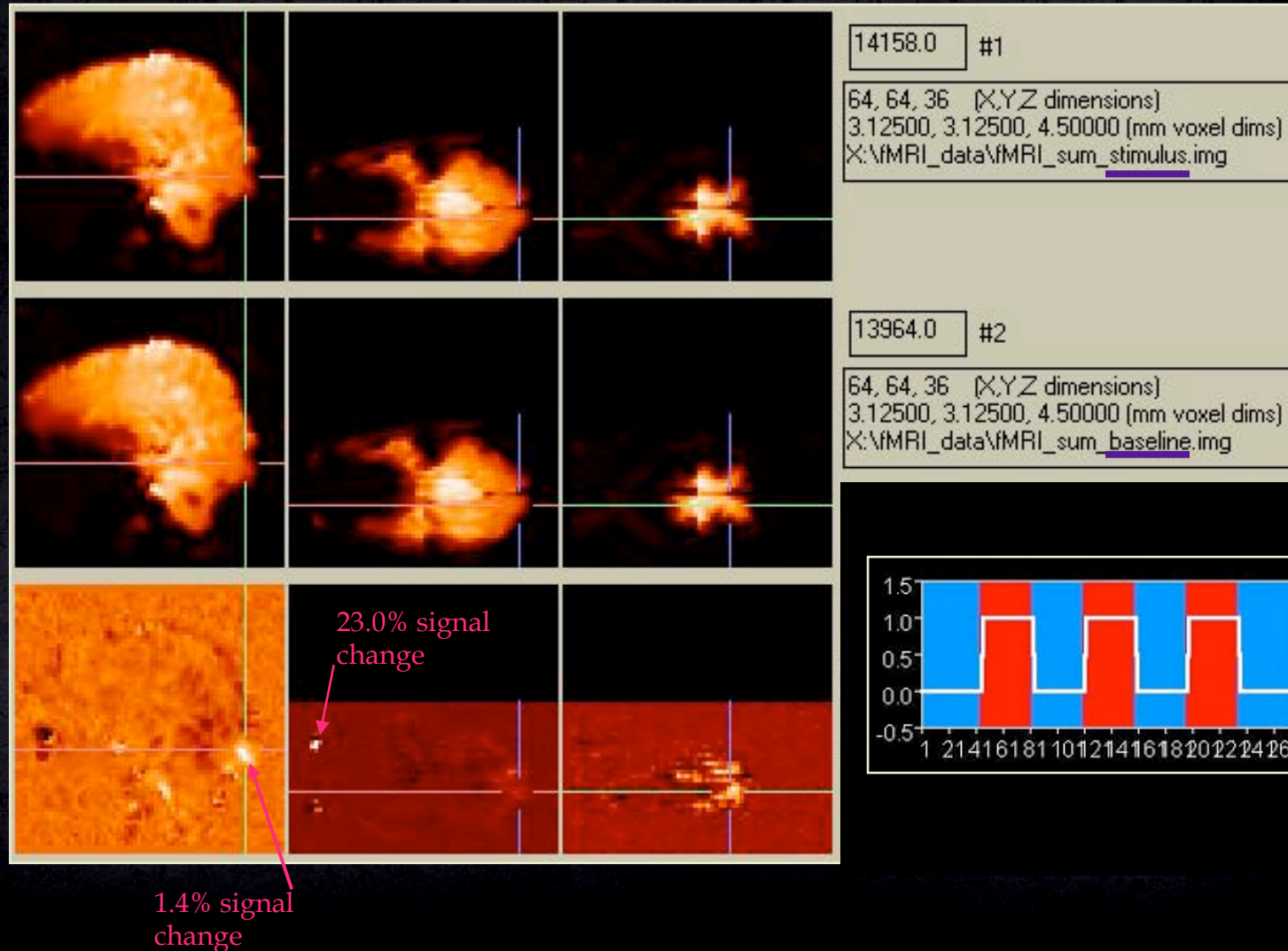
To Wisconsin Badger fans,  
the brain obscures the logo.

An artifact is anything that prevents you  
from seeing what you want to see.

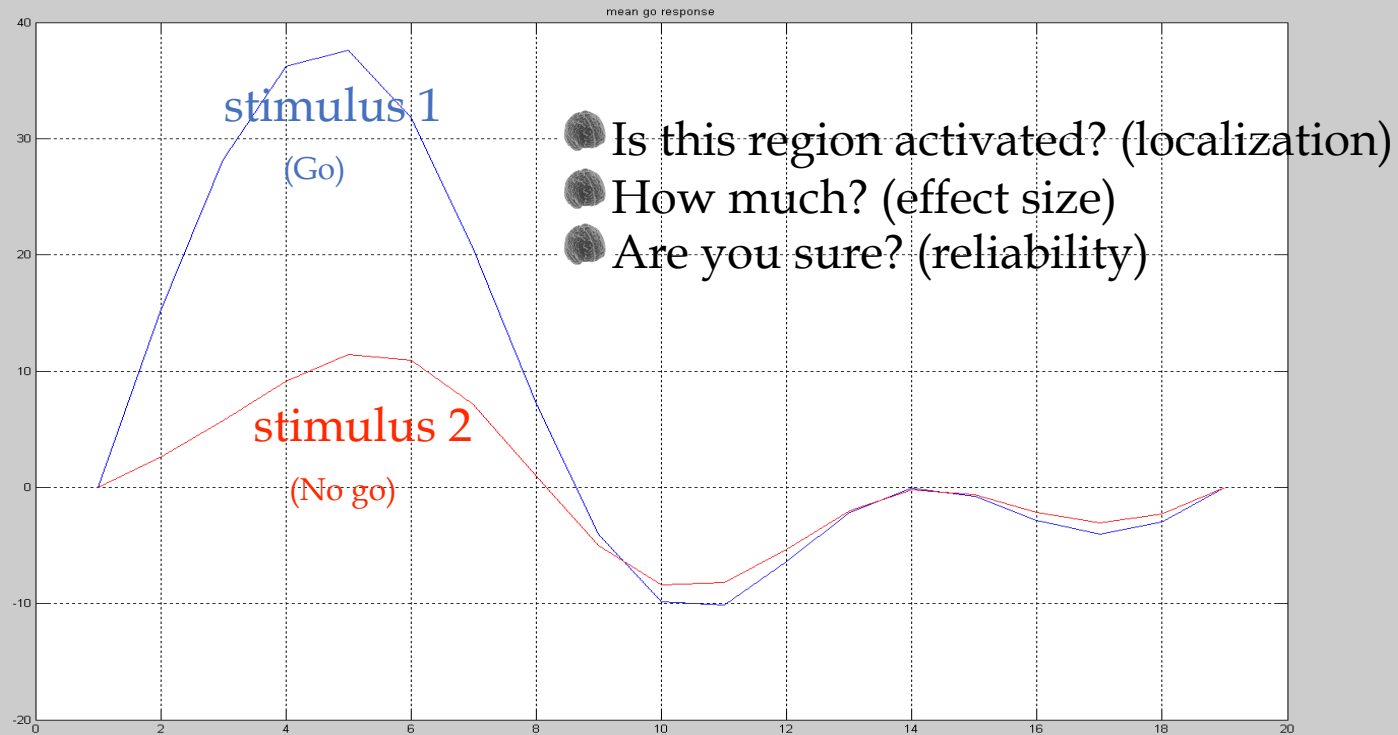
# What is the Signal?



# What is the goal?



# Big-picture goal










# Artifact Sources

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$$t = \frac{\text{effect}}{\text{variance}}$$








## Physiological

-  cardiac, respiratory motion
-  subject movement
-  poor intersubject alignment
-  B-field susceptibility (dropout)
-  foreign objects



## Scanner

-  SNR
-  B-field inhomogeneity
-  detector coil sensitivity
-  reconstruction tradeoffs
-  slice-timing (2D) effects



# A Scientific Experiment

## 🧠 Before

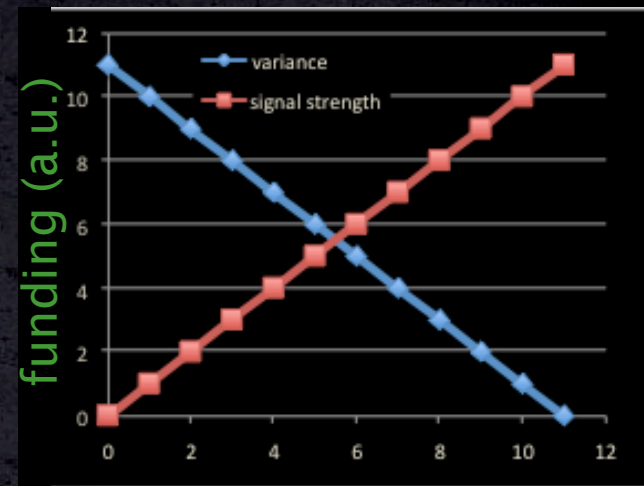
- 🧠 measure twice, cut once

## 🧠 During

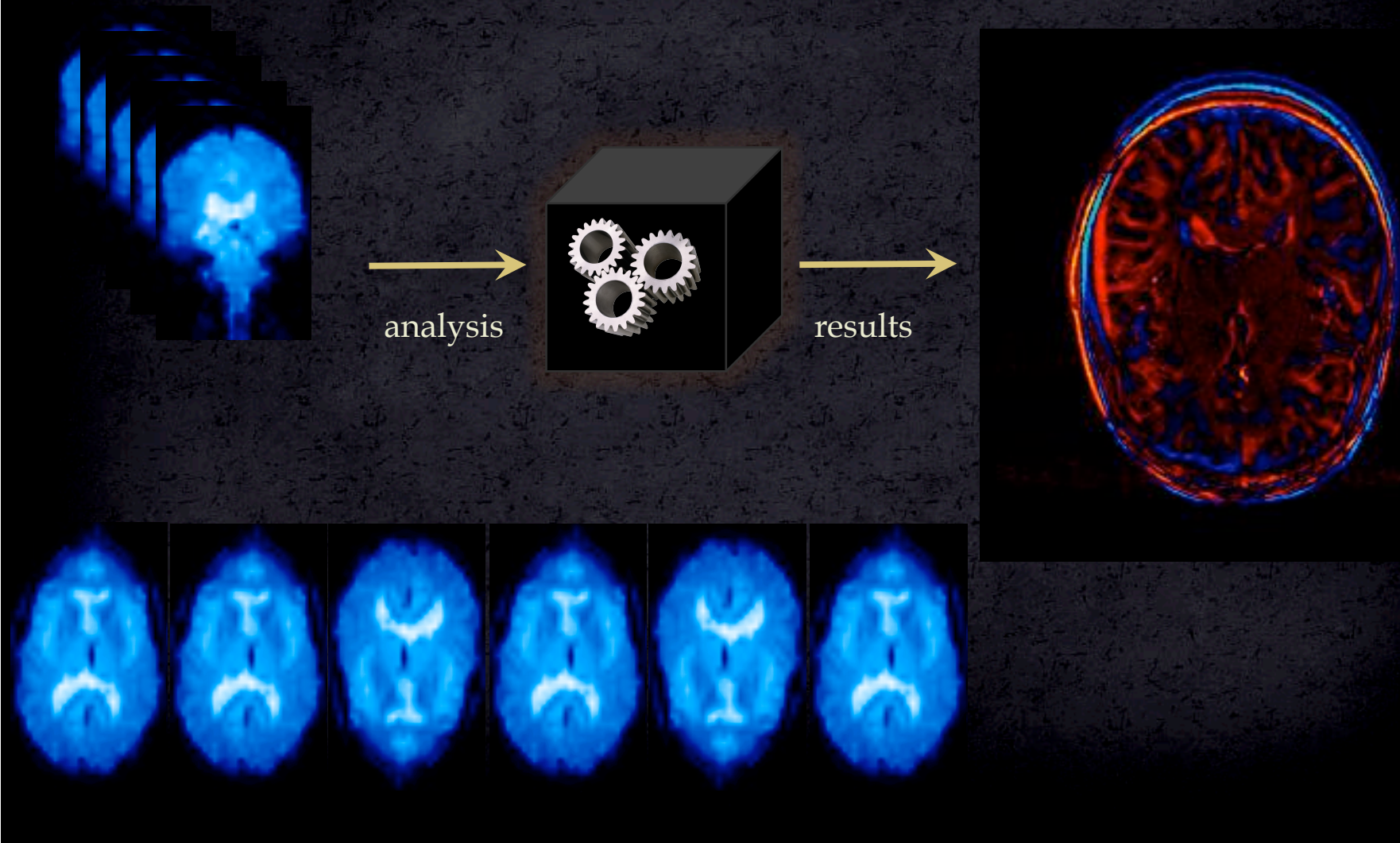
- 🧠 look at your data. with your eyes.

## 🧠 After

- 🧠 pre-processing: modeling and removing variance
- 🧠 data analysis: modeling and discovering signal



# The single biggest artifact source





# Being Clever Ahead of Time

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## Before



Learn a package

- provides an orderly introduction to analysis.



Software programming skills



File format conversion



Experimental paradigm

- event-related paradigms can isolate stimulus, HR



Acquisition sequence



Collect enough data

- multispectral anatomicals (T1, T2, PD, ...)
- field map
- physiological (cardiac, respiratory, skin conductance, eye tracking)
- estimator for HRF (e.g. motor response)

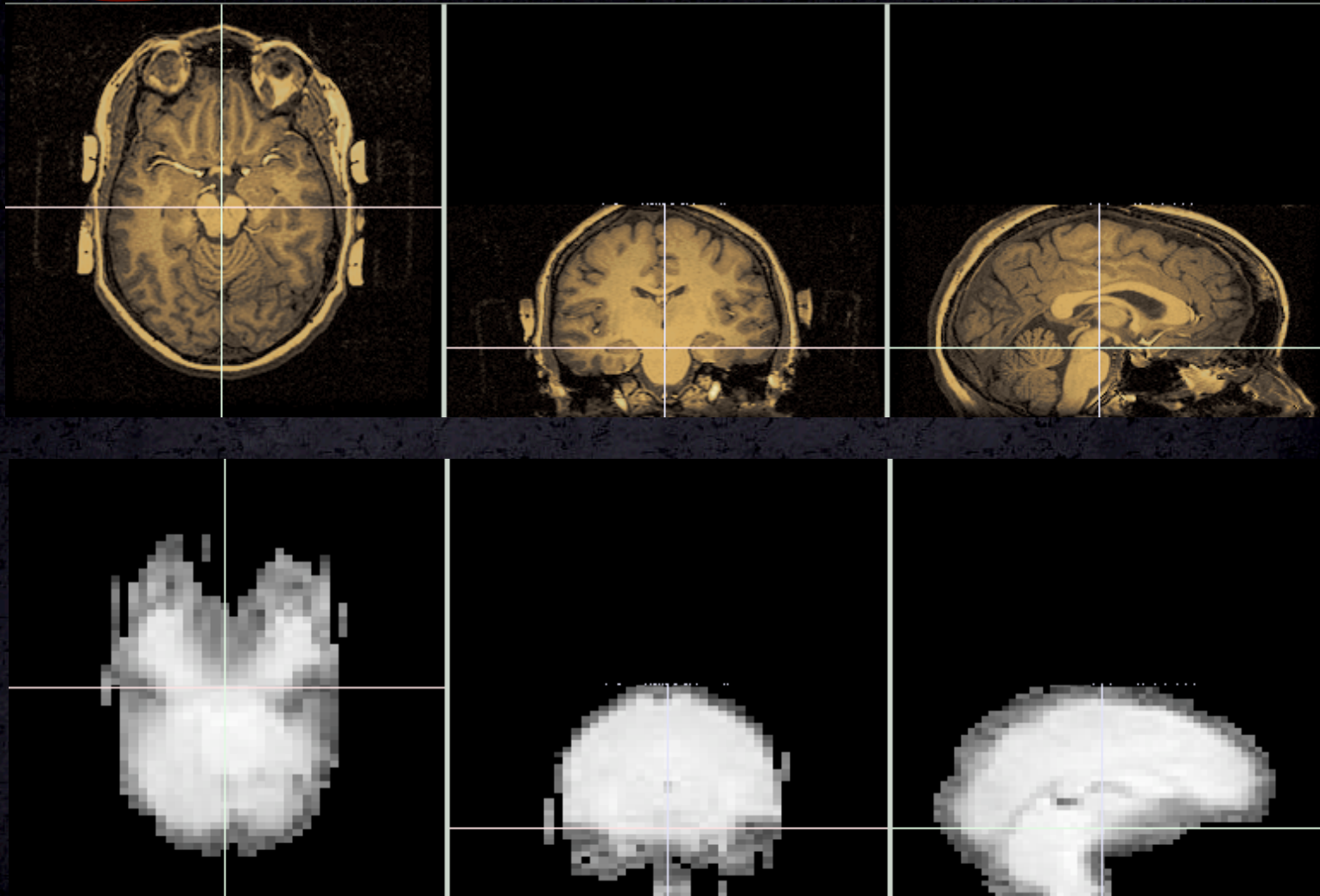


# Post-hoc Corrections

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- Some folks call it image processing...
  - spatial registration
  - field map correction
  - slice time correction
  - motion correction
  - smoothing- spatial, temporal
- These corrections are ignorant of the experimental model.

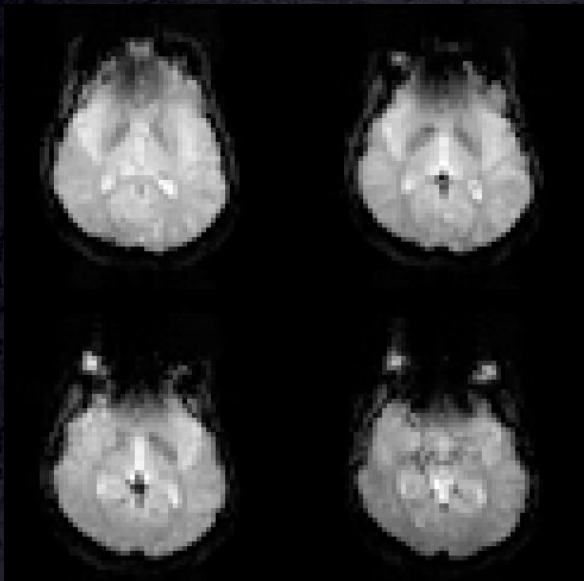
# EPI Dropout (susceptibility) artifact



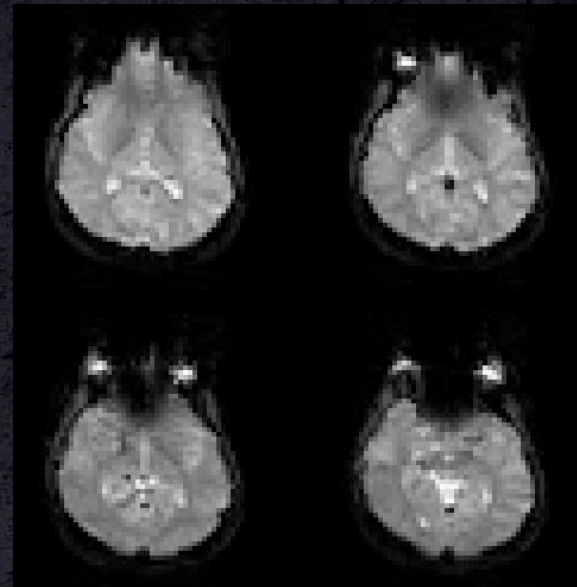
phase dispersion => signal loss

# EPI susceptibility artifact

clever ahead of time: optimize acquisition parameters



TE = 30 ms  
4mm thick slices

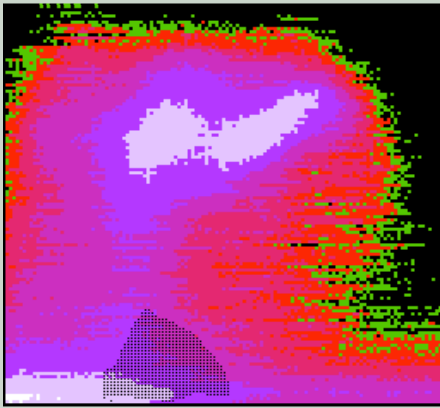


TE = 20 ms  
2mm thick slices

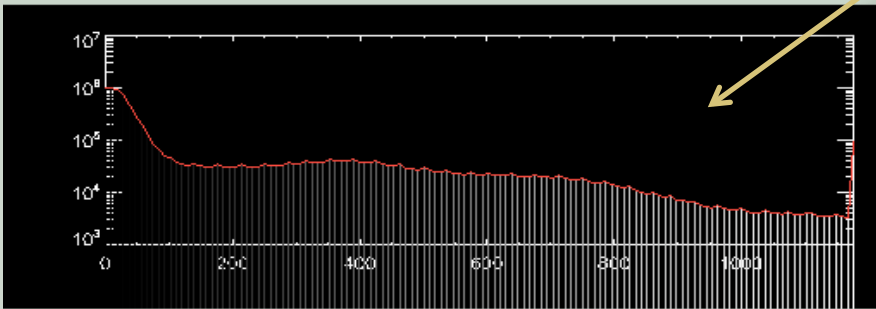
courtesy of Andy Alexander

EPI

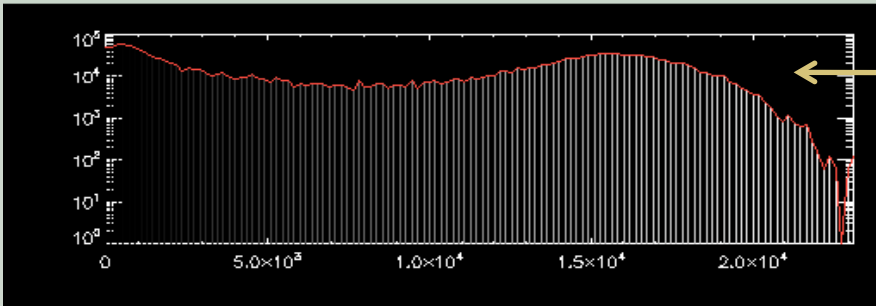
HistoMulti Display



T1

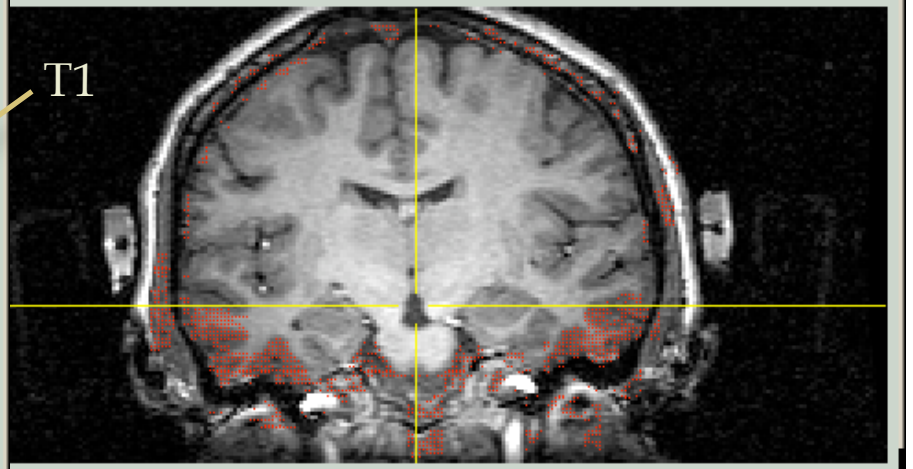


Y-Axis log [Lop Top](#) [Help](#)

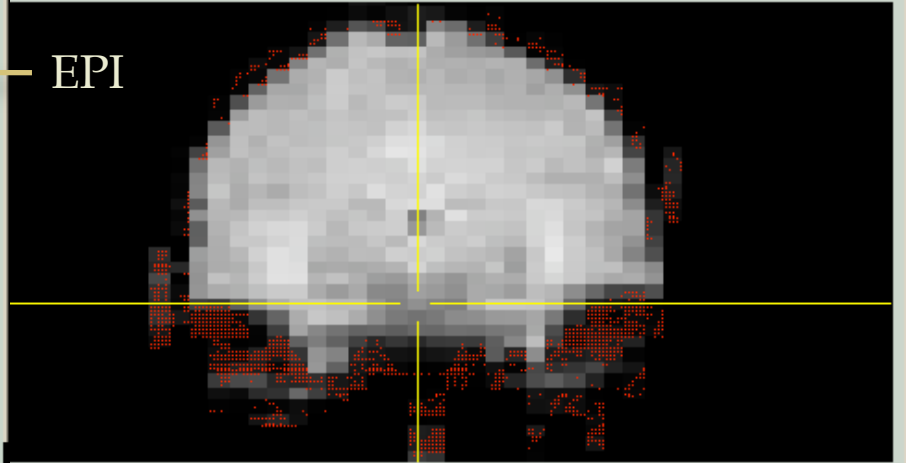


EPI dropout artifact

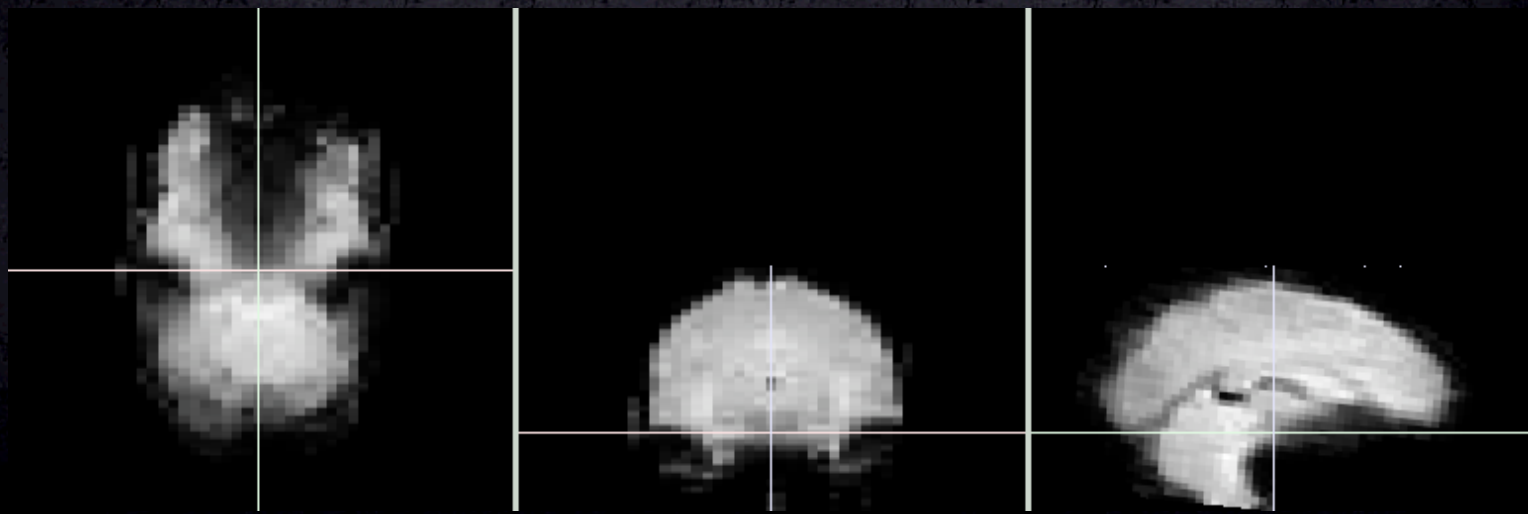
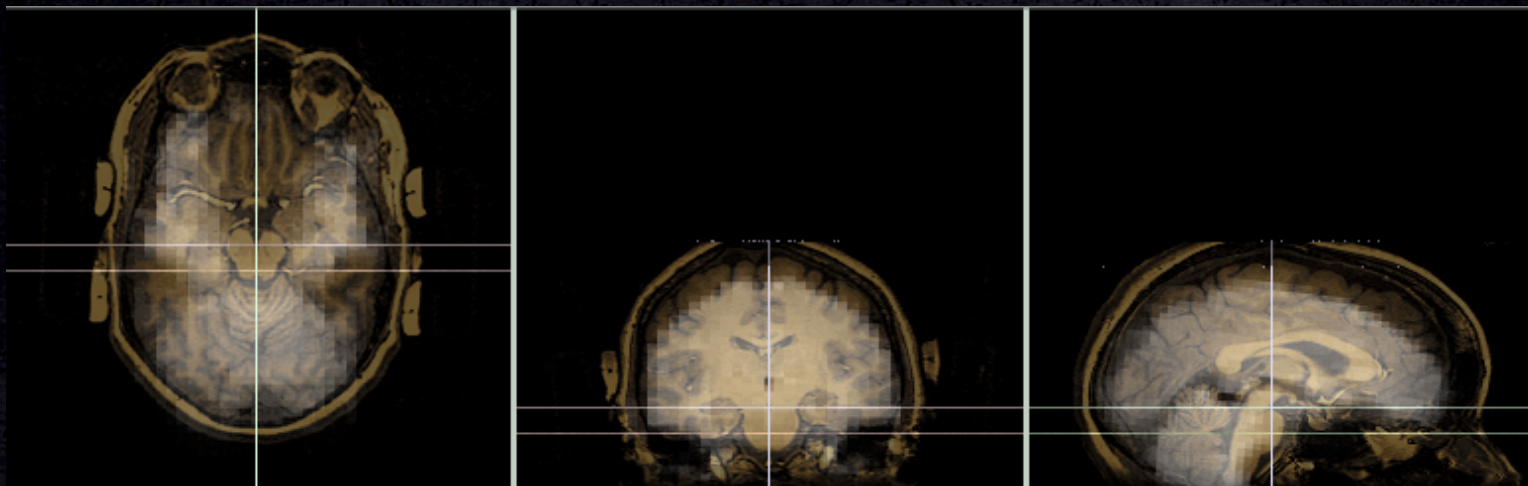
Slice Display: Coronal



ronal

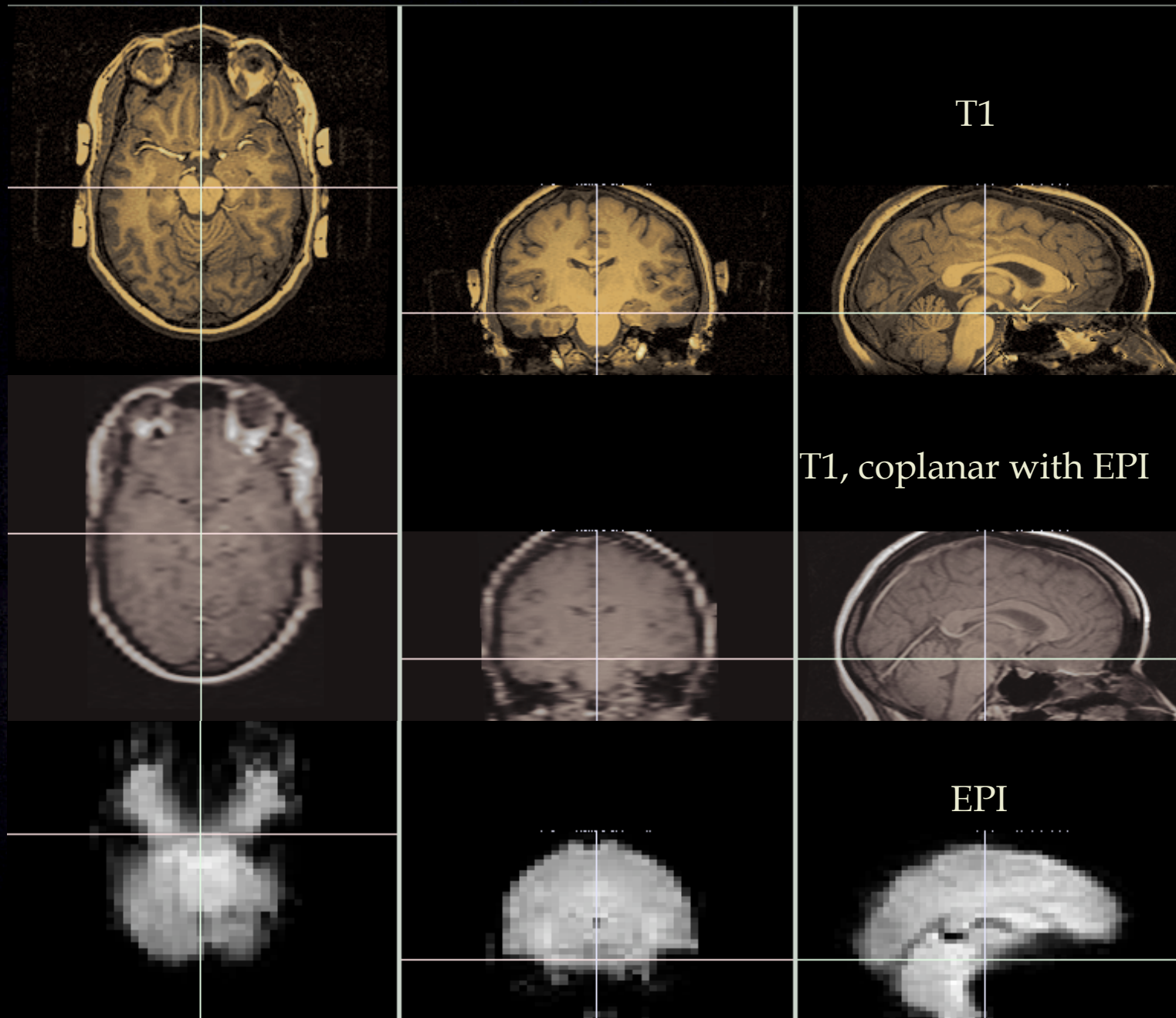


# EPI registration - tread carefully





# EPI registration: indirect approach



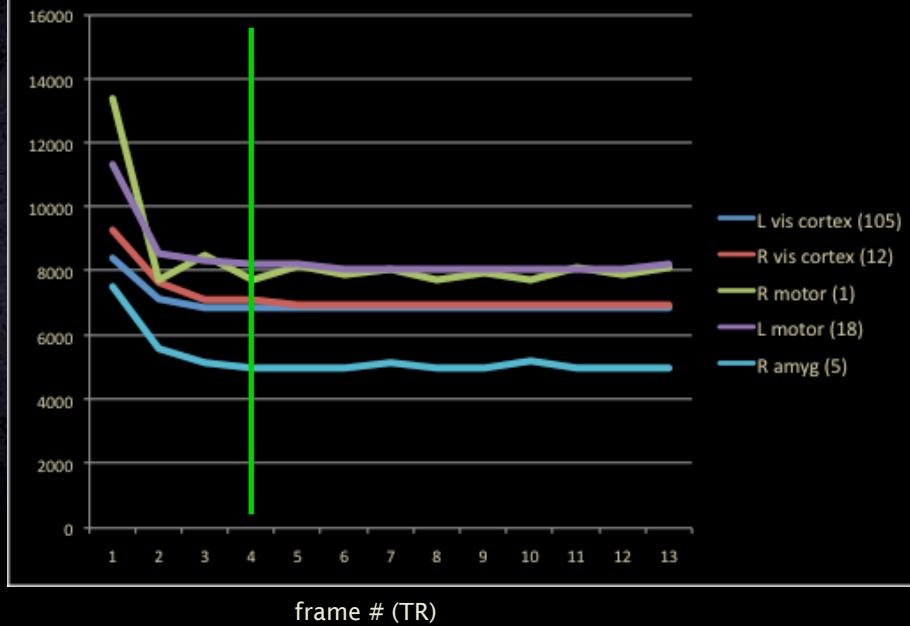
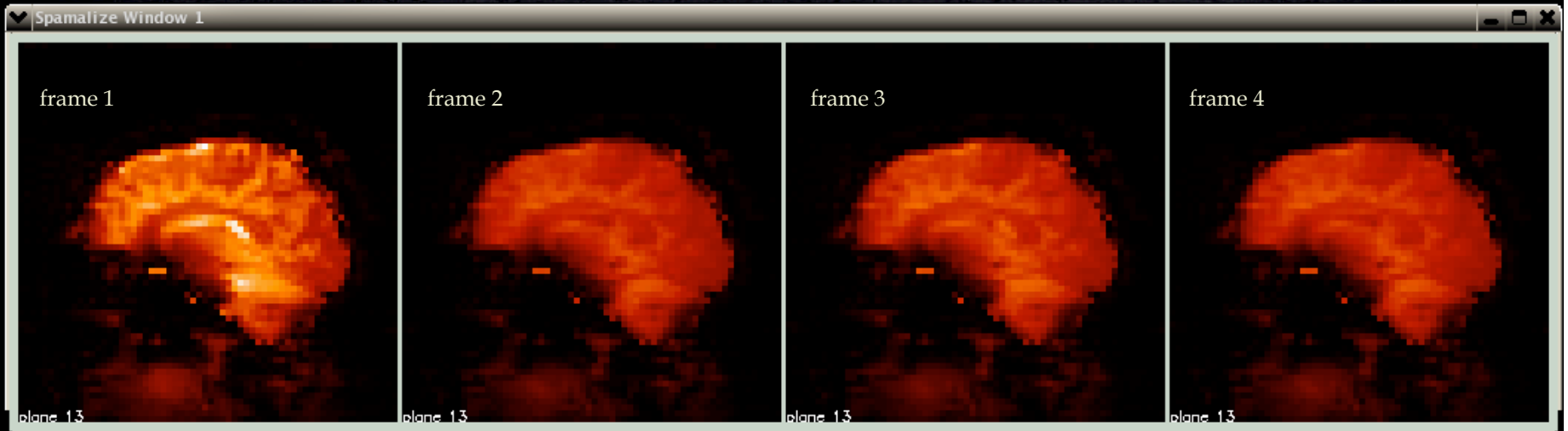
register

assume  
no  
movement

# Typical acquisition sequence



# Off to a bad start



Remove first 3-5 frames:

● delete from series

or

● mark via GLM software

or

● assign to a unique condition



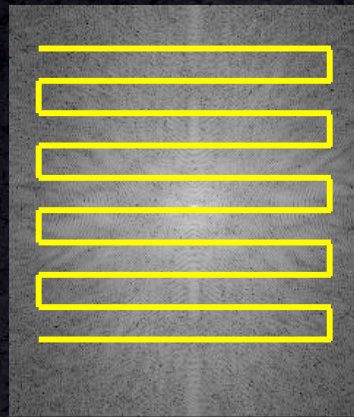
# Field Map Correction

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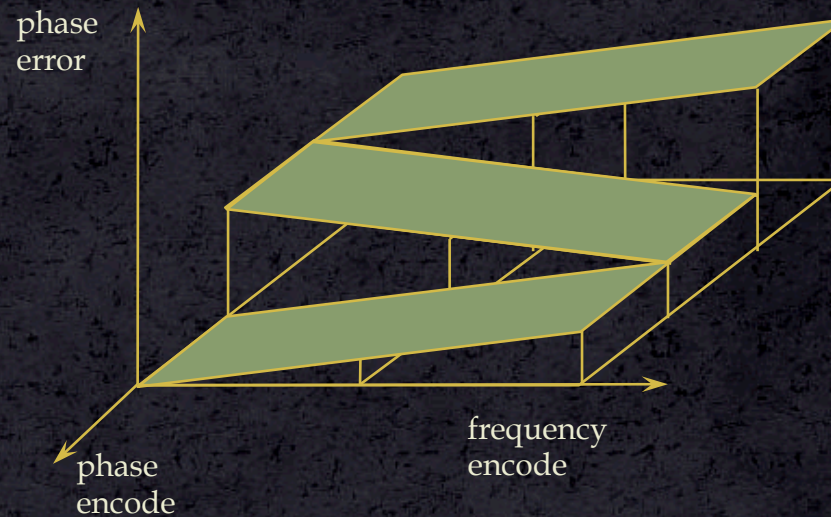
- The magnetic field is not uniform, leading to misplaced signal, since recording/reconstruction assumes a uniform gradient.
- 3T => worse
- Nonuniformities are object-dependent.
- Largest source of  $B_0$  inhomogeneity:  
air-tissue interfaces => susceptibility differences
- Different acquisition sequences may have different affect.
  - EPI data (Gradient Echo) most affected (fMRI, DTI)
  - Spin Echo affected little
- Luckily, this can be modeled and corrected...
  - But, a separate measurement is required.
  - 2 scans with different TEs (e.g. 8, 11 msec), minimal distortion.

# B-Field Distortion

## The Cause: EPI Phase Error Accumulation

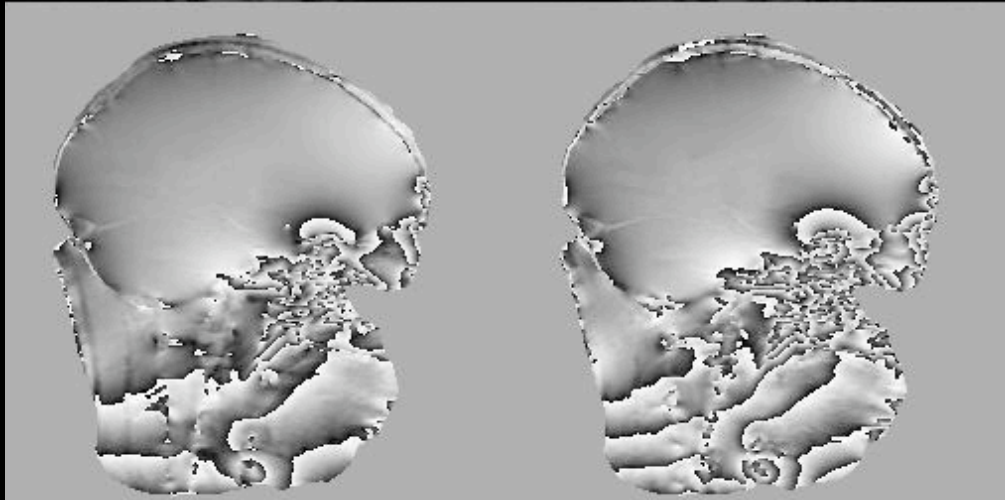
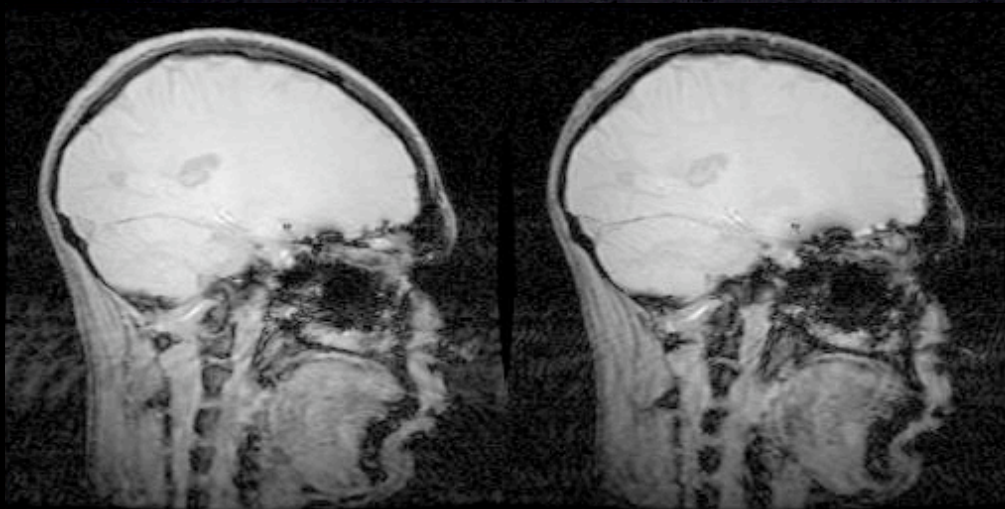


k-space



- For a linear field offset, phase error accumulates linearly.
- Cummulative phase errors cause a shift in position

# Distortion (Fieldmap) Correction



TE=7ms

TE=10ms

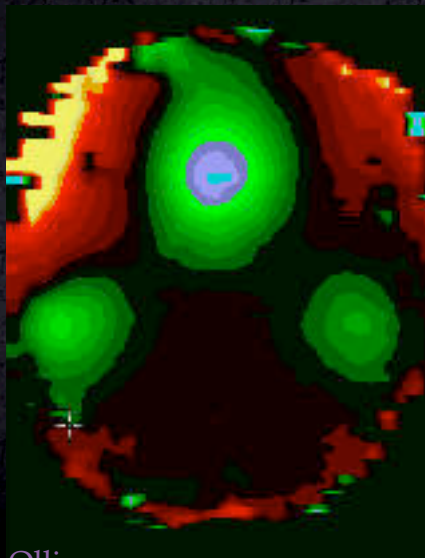
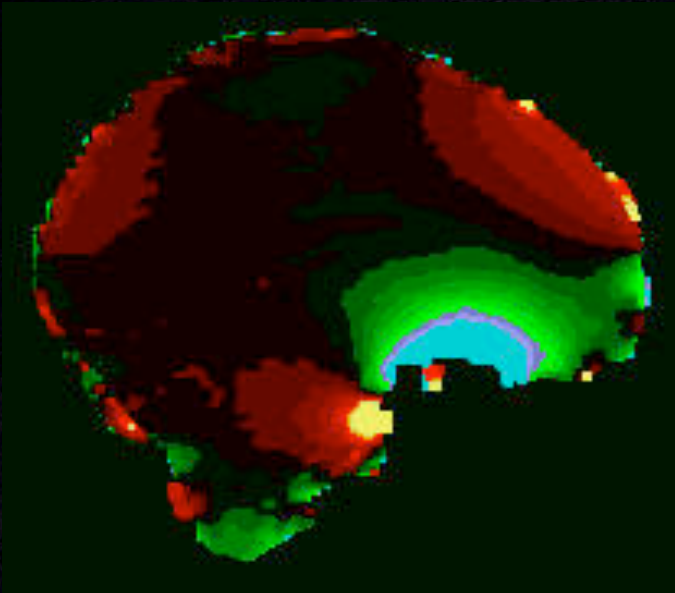
- Strategy: Collect two gradient echo images at short but different echo times.
- Unwrap the phase.
- Phase-difference proportional to the pixel-offset along the phase-encode axis.
- Resample the EPI image to correct for the offset.

Peter Jezzard and Stuart Clare, "Sources of distortion in functional MRI data", *Human Brain Mapping*, 8:80-85, 1995.

courtesy of John Ollinger

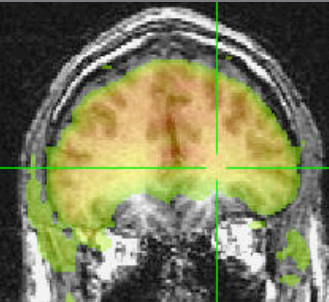
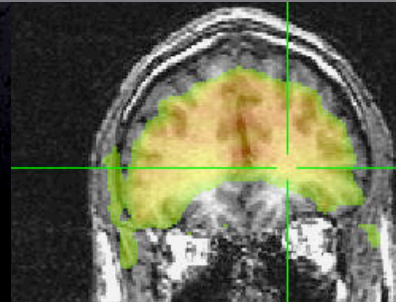
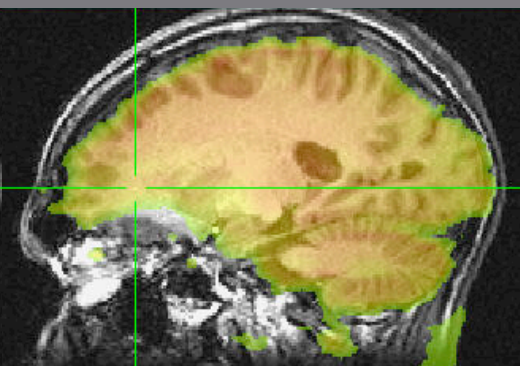
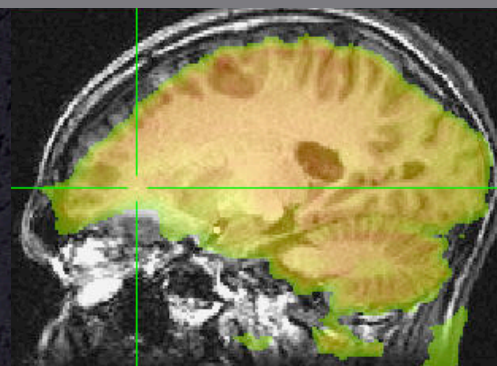
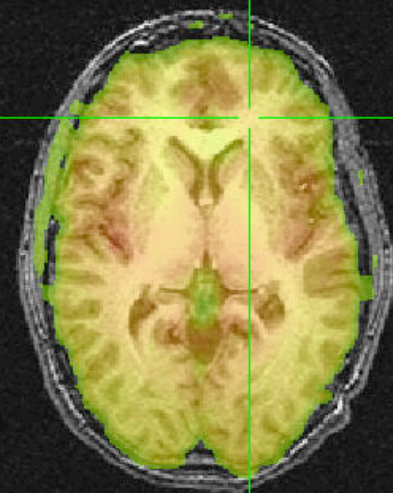
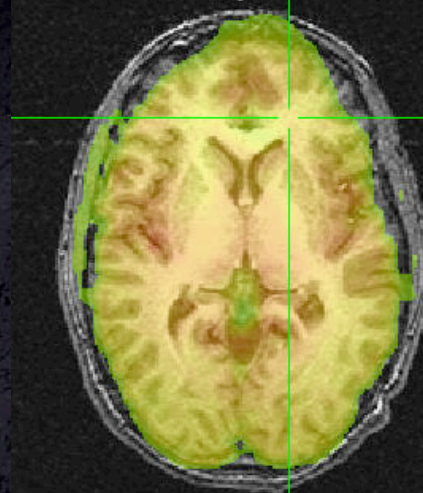
# Field Map Correction

pixel  
shift



original

FM corrected



courtesy of John Ollinger



# Field Map Correction

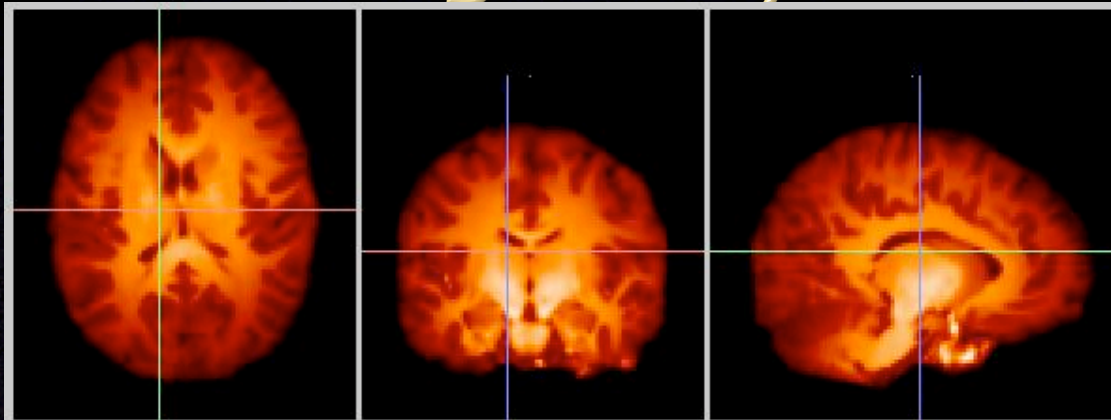
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- Magnitude of correction depends on the magnitude of the susceptibility artifact, which depends on the size of the sinuses.
  - Larger in men than women.
  - Larger in adults than children
- Although the magnitude of the correction is often small, it can reduce confounds between gender, age and susceptibility.
- It cannot recover missing data from the dropout region.

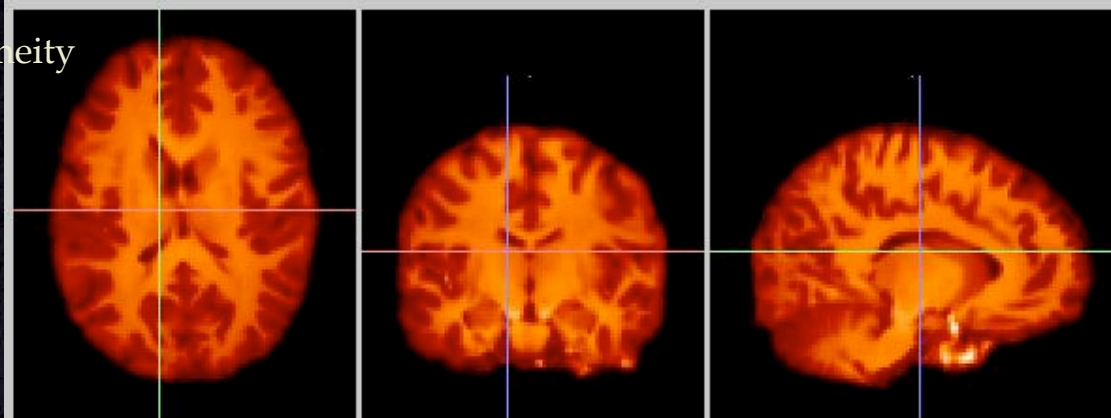


# Inhomogeneity Correction

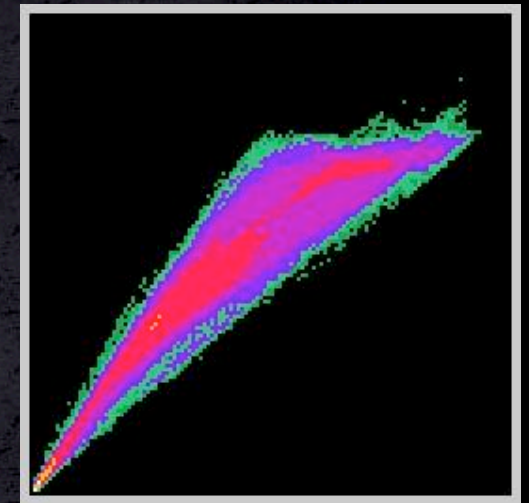
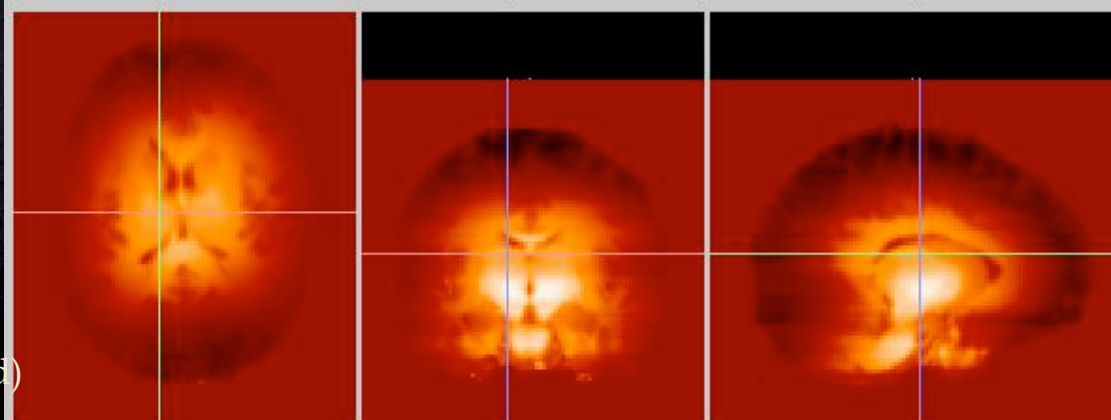
original



inhomogeneity corrected



Difference  
(~ bias field)



joint histogram

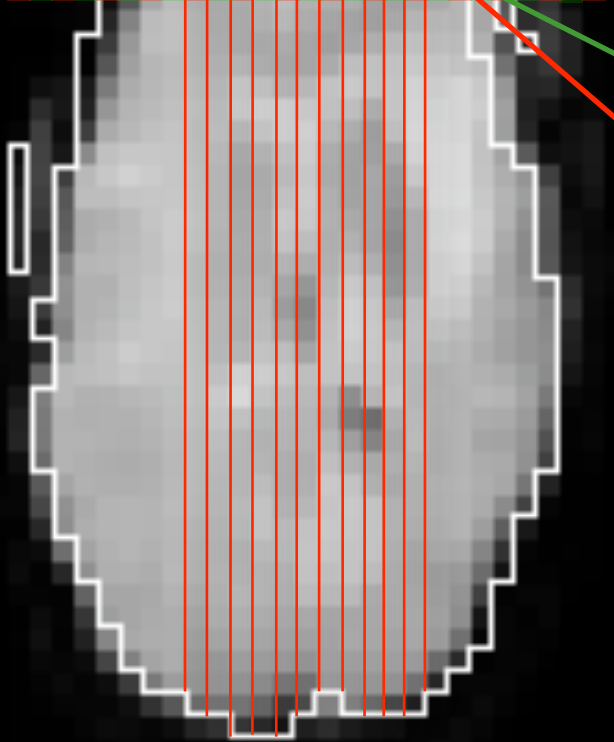
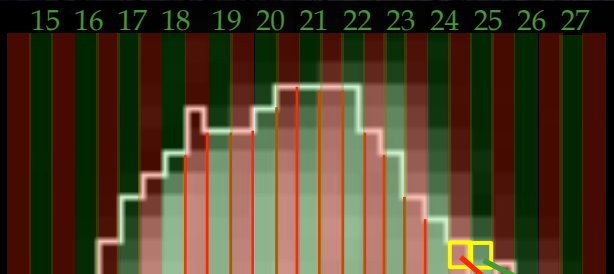
# Inhomogeneity Correction

- Increase gradient magnetic field strength.
- Decrease echo time.
- Smaller pixels (better resolution).
- Phase encoding.
- Postprocessing.



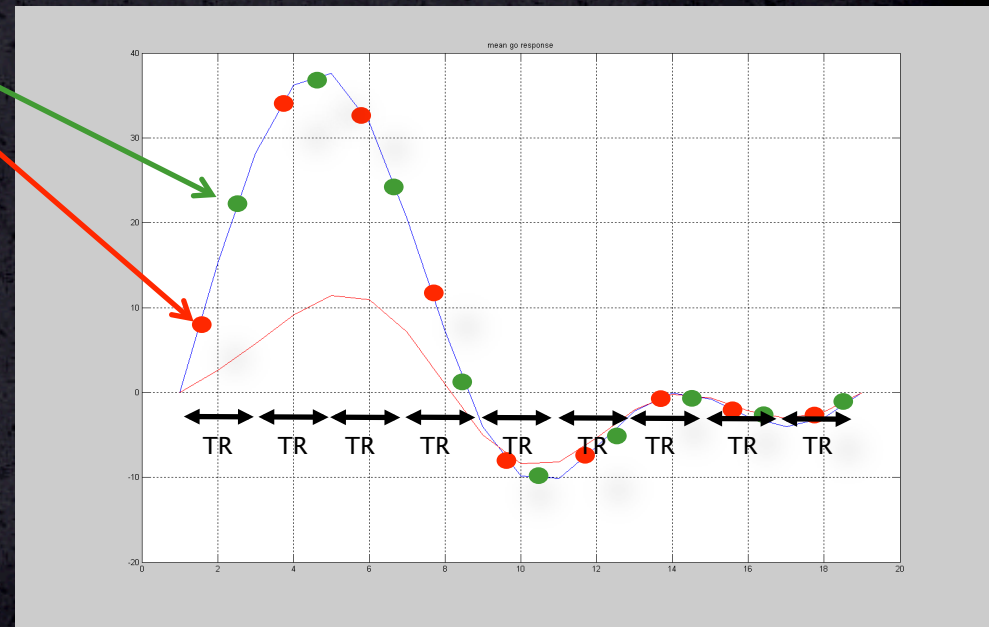
# Slice-time Correction

1 2 3 4 5 6 7 8 9 10 11 12 13 14  
15 16 17 18 19 20 21 22 23 24 25 26 27



Make all slices appear to have been acquired at the same time.

A "reference" HRF should look the same in all slices.



More important for longer TR.  
Usually best prior to motion correction.



# Motion Artifacts

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## Sources

- Subject motion
- Peripheral movement (changes B-field)
- Respiration, cardiac



## Magnitude / Importance

- a significant fraction of the fMRI signal!



## Model

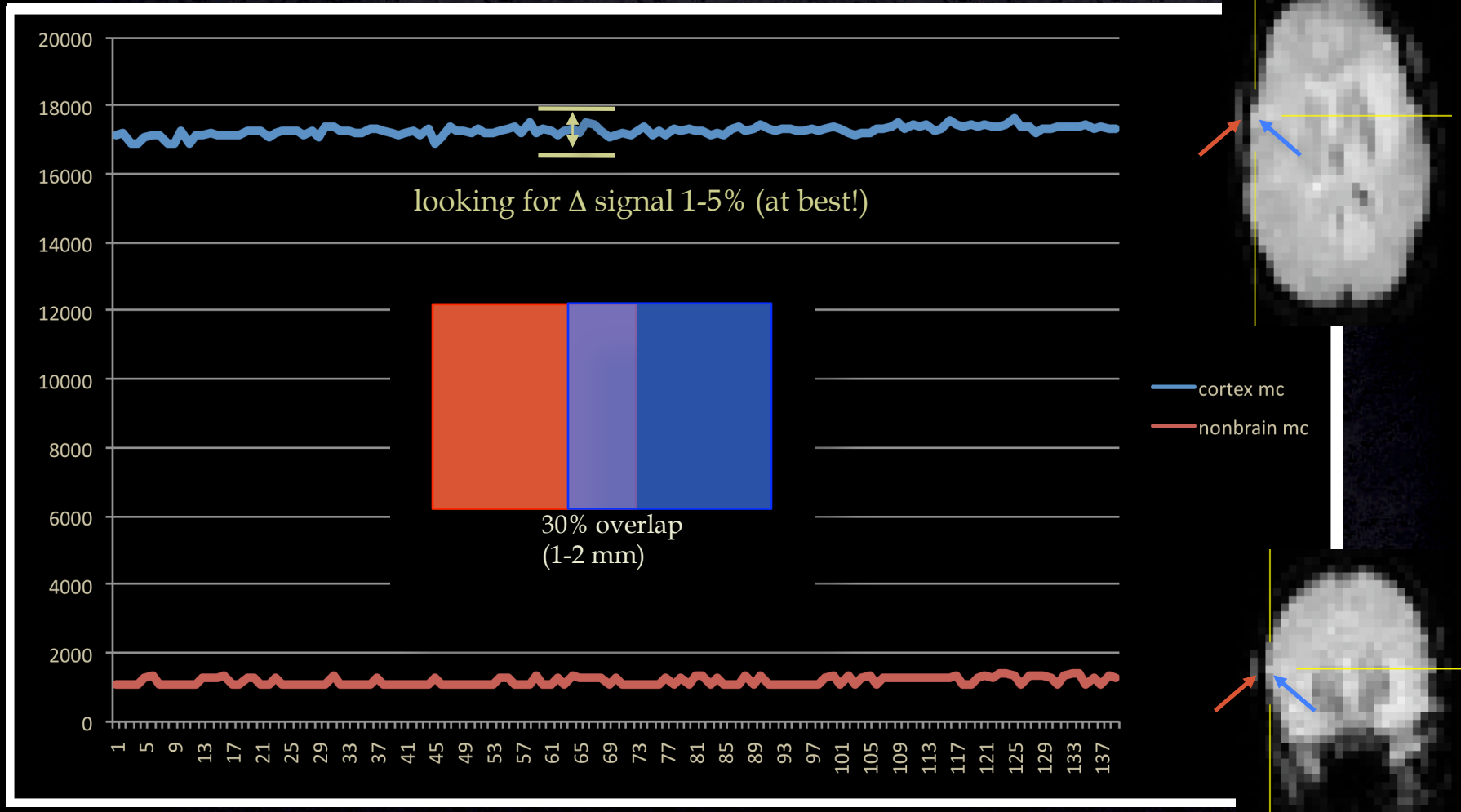
- framewise 3D volumetric
  - rigid body (translation, rotation)
  - ignores intraframe motion
- assumes only small movement



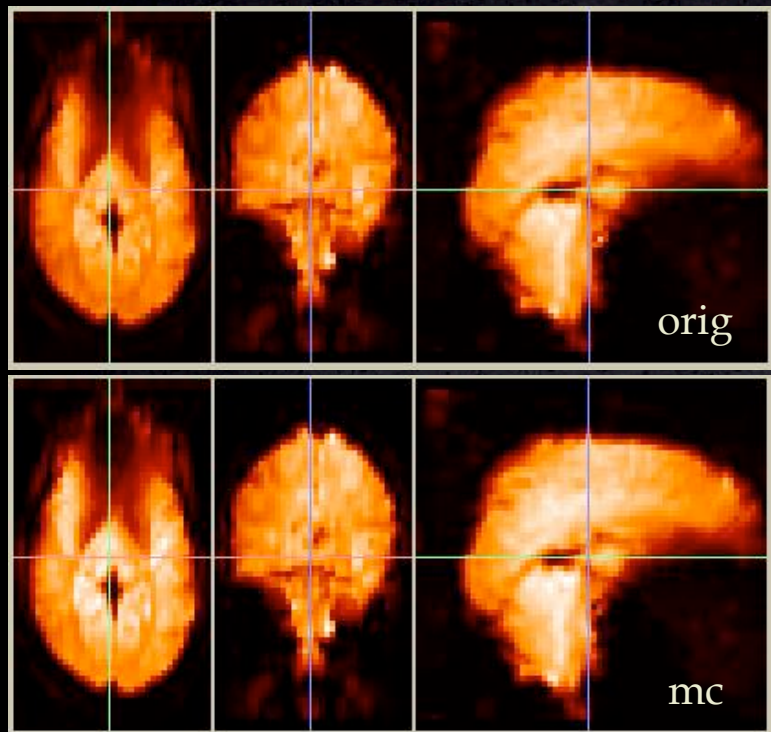
## Correlation between motion, stimulus

- correcting motion can attenuate activation signal
- motion estimates can be incorporated into GLM

# Motion Correction: Magnitude



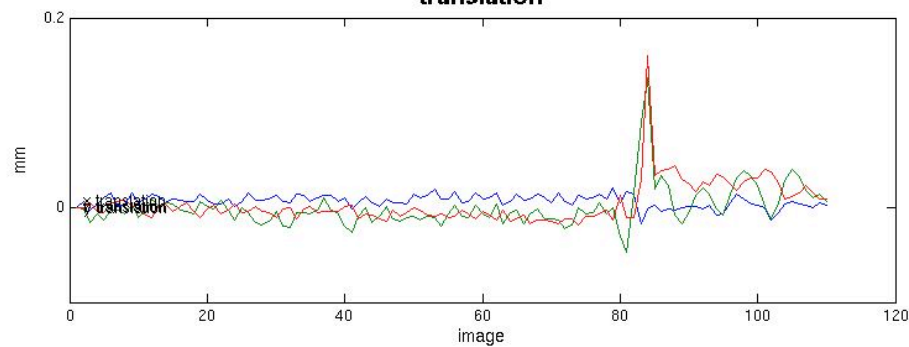
# Motion Correction



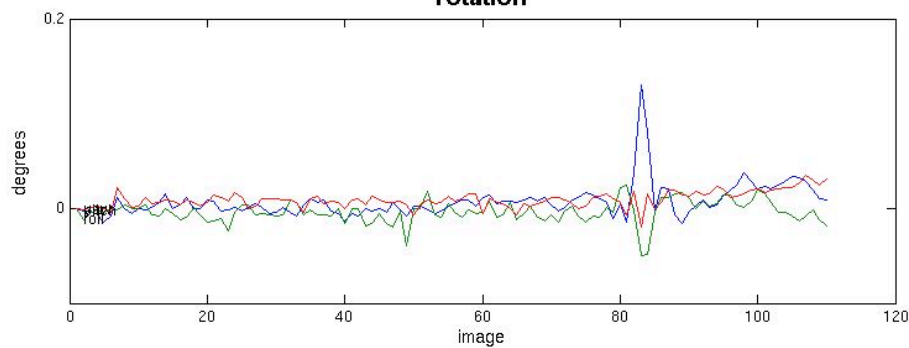
## Image realignment

- 1 /scratch/MRI\_data/data/fMRI\_vis\_stim\_0000.img
- 2 /scratch/MRI\_data/data/fMRI\_vis\_stim\_0001.img
- 3 /scratch/MRI\_data/data/fMRI\_vis\_stim\_0002.img
- 4 /scratch/MRI\_data/data/fMRI\_vis\_stim\_0003.img
- 5 /scratch/MRI\_data/data/fMRI\_vis\_stim\_0004.img
- 6 /scratch/MRI\_data/data/fMRI\_vis\_stim\_0005.img
- 7 /scratch/MRI\_data/data/fMRI\_vis\_stim\_0006.img
- 8 /scratch/MRI\_data/data/fMRI\_vis\_stim\_0007.img
- 9 /scratch/MRI\_data/data/fMRI\_vis\_stim\_0008.img
- 10 /scratch/MRI\_data/data/fMRI\_vis\_stim\_0009.img
- 11 /scratch/MRI\_data/data/fMRI\_vis\_stim\_0010.img
- 12 /scratch/MRI\_data/data/fMRI\_vis\_stim\_0011.img
- ..... etc

## translation



## rotation

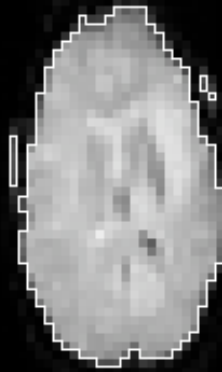
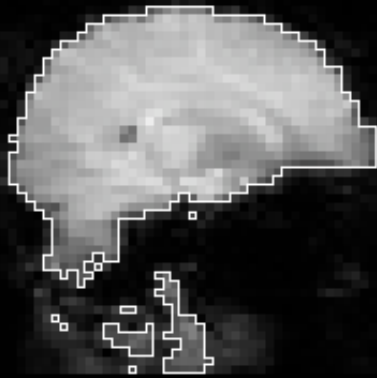


# Motion Correction: Subject Motion

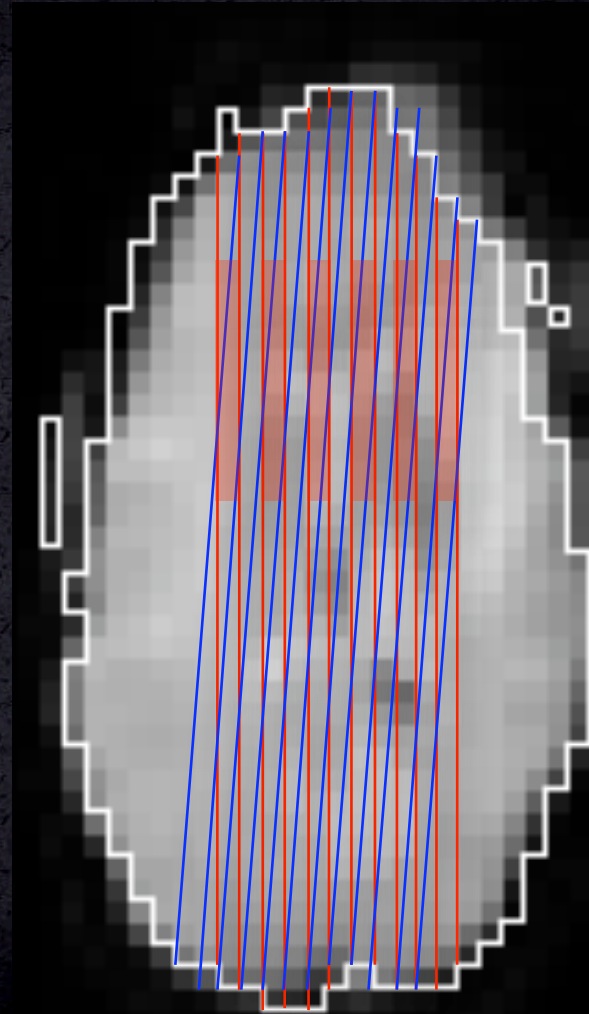
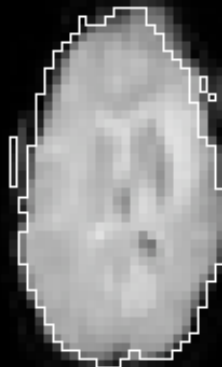
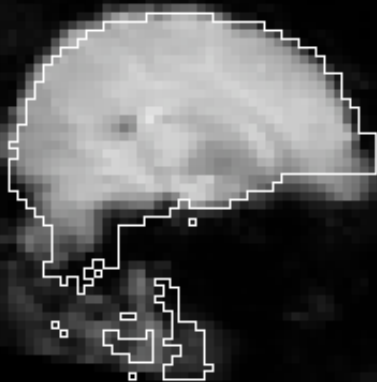
in-plane motion: easy

between-plane: messy

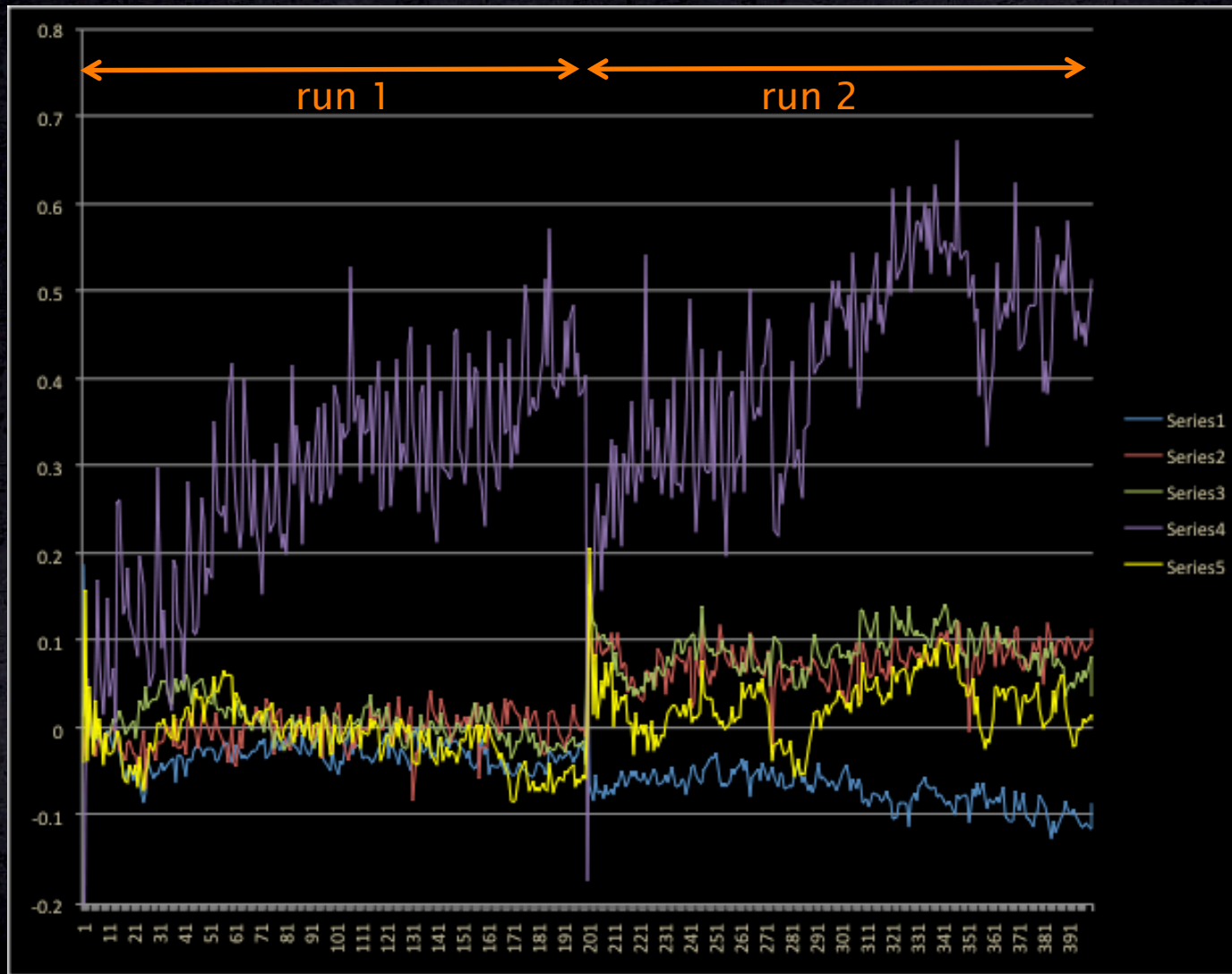
t=0



t=later



# Combining scan runs





# Motion Artifact: Typical pattern

Single subject data

axial

A

P

effect size



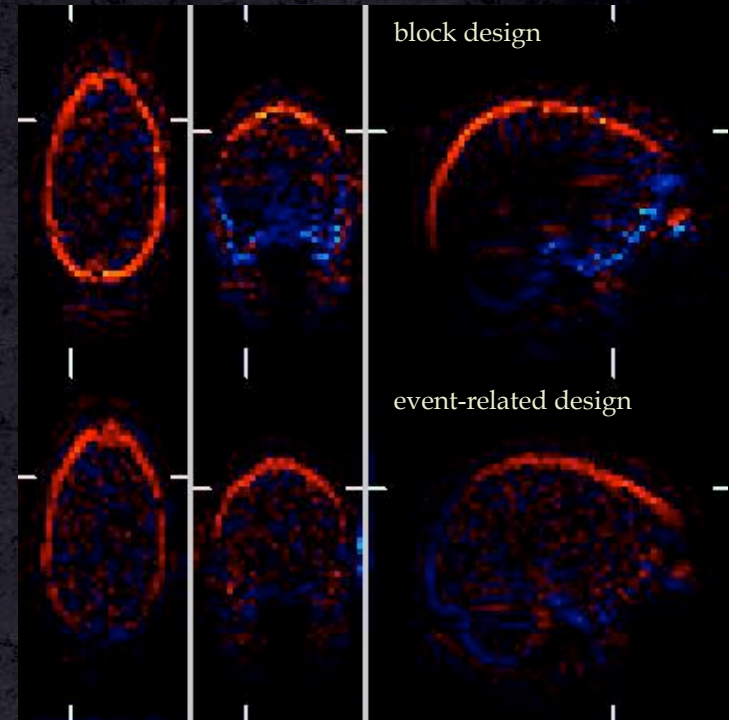
coronal

original

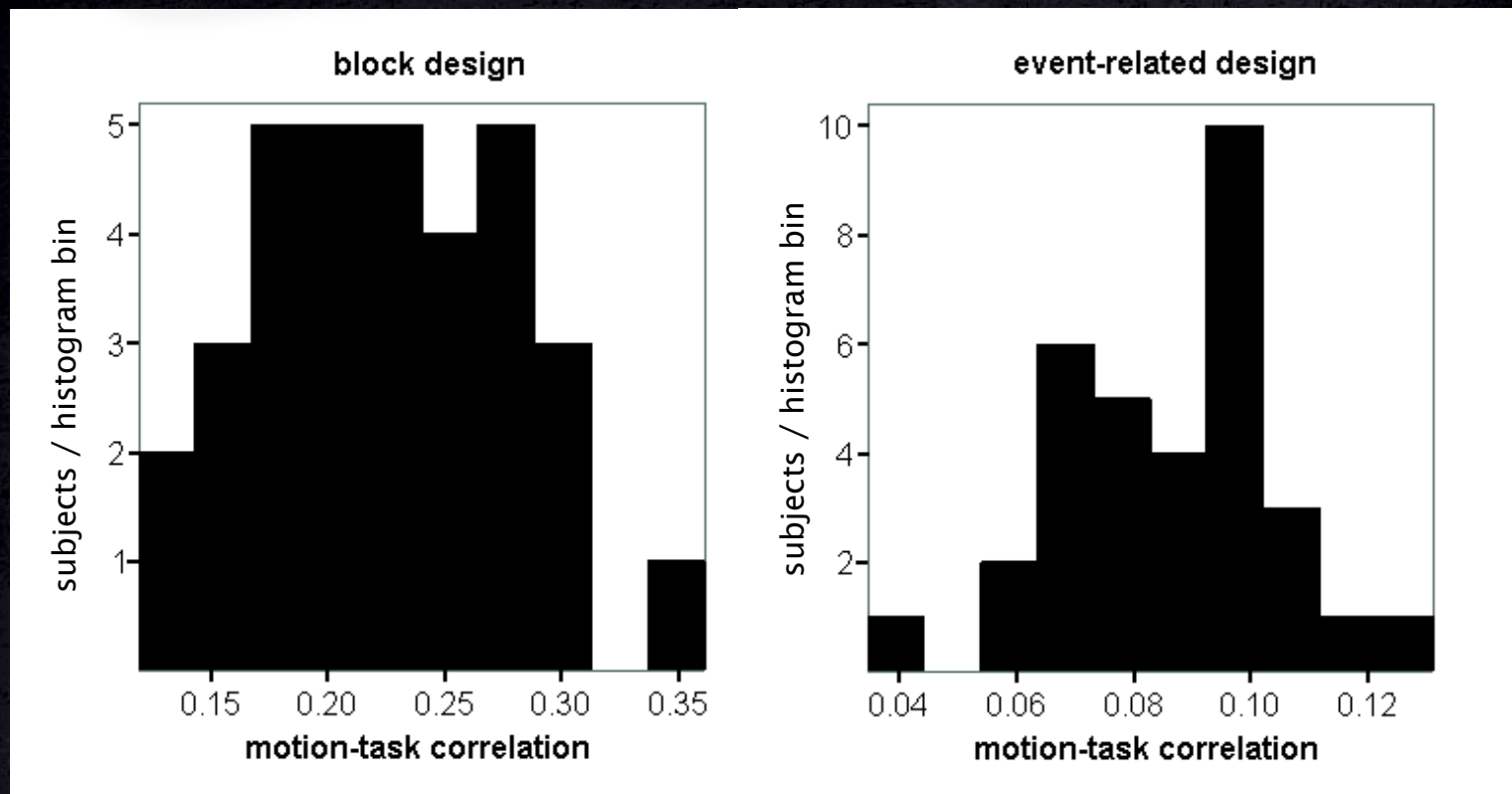
motion corrected

S

I



# Motion Correlated with Stimulus



Johnstone T et al., "Motion Correction and the Use of Motion Covariates in Multiple-Subject fMRI Analysis", *Hum Brain Mapp* 27:779 -788, 2006.  
Birn RM et al., "Event-related fMRI of tasks involving brief motion", *Hum Brain Mapp* 7:106 - 114, 1999.



# Motion Parameters:

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
How can we use this information for Good?

 Apply motion correction: reslice each 3D volume

 “standard” approach

 loss of sensitivity if motion correlated with activation

 Use parameters as covariates in GLM

 may increase sensitivity

 more flexible data analysis

 small loss of degrees of freedom in GLM

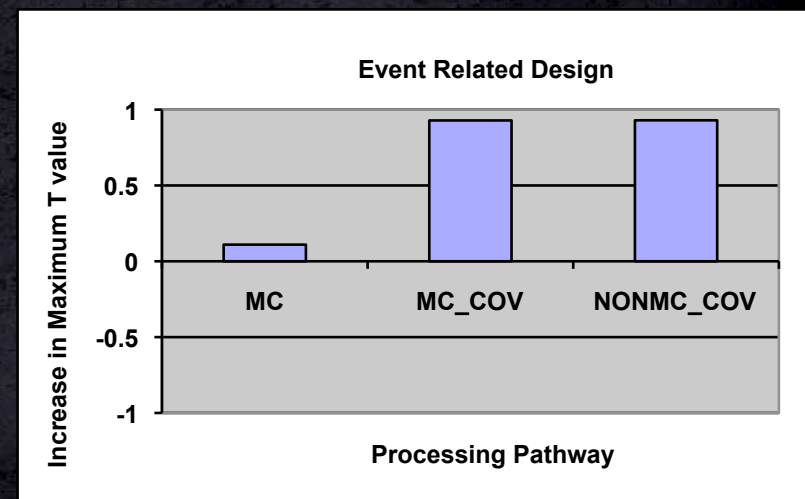
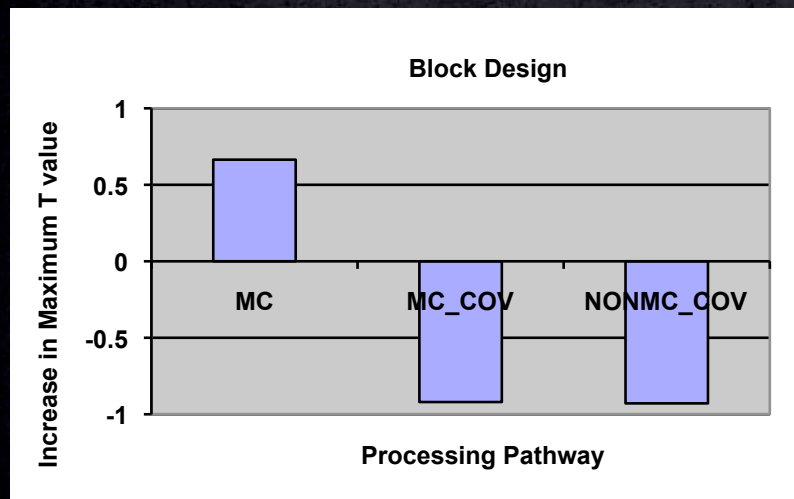
# Motion Parameters as GLM Covariates

🧠 Block design:

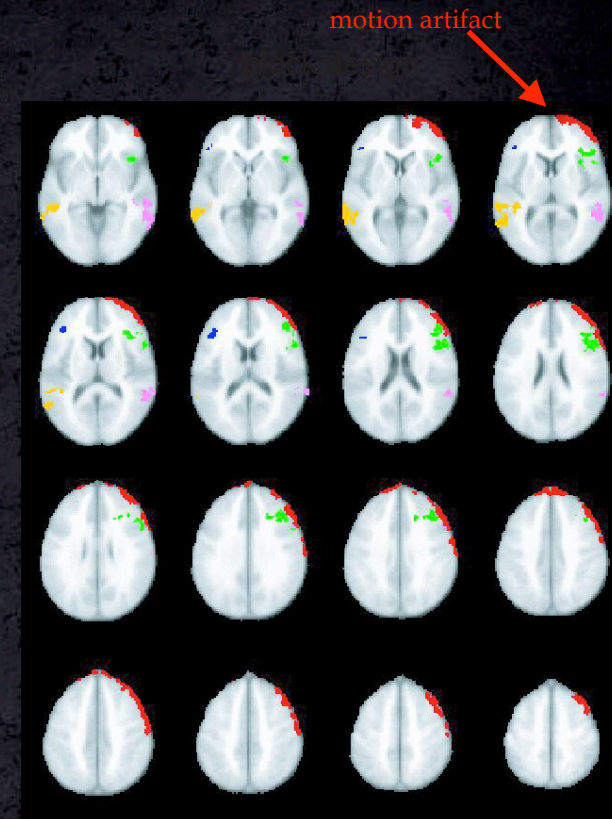
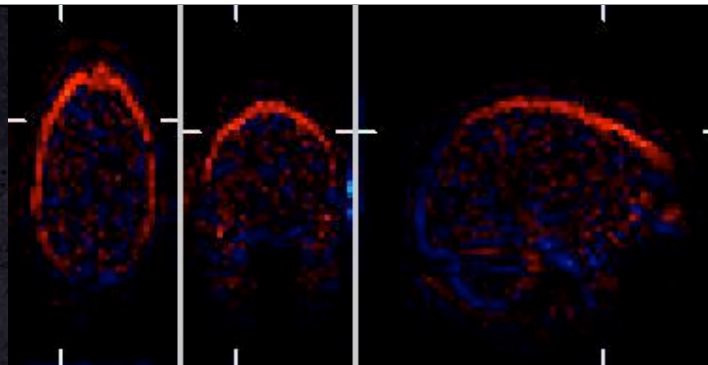
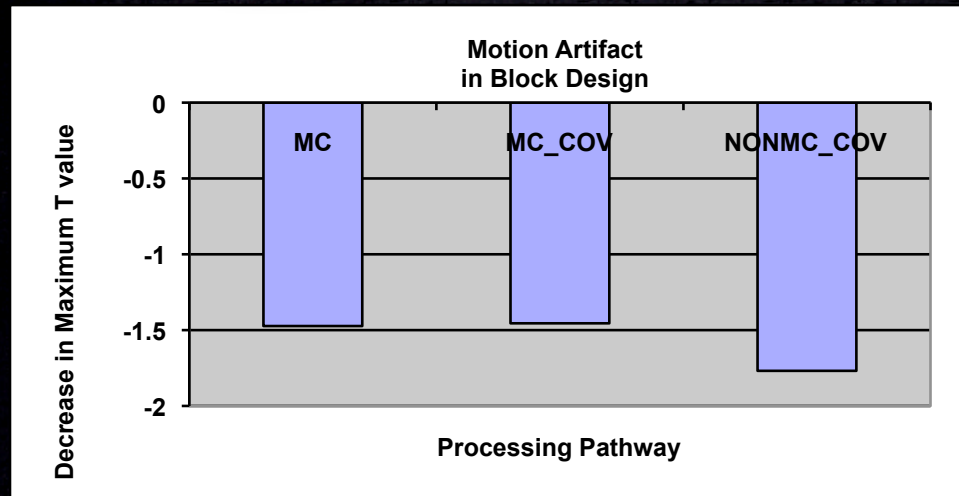
🧠 if motion correlated with stimulus, “standard” reslice best

🧠 Event-related design:

🧠 motion parameters in GLM usually work well.



# Motion Correction at Work



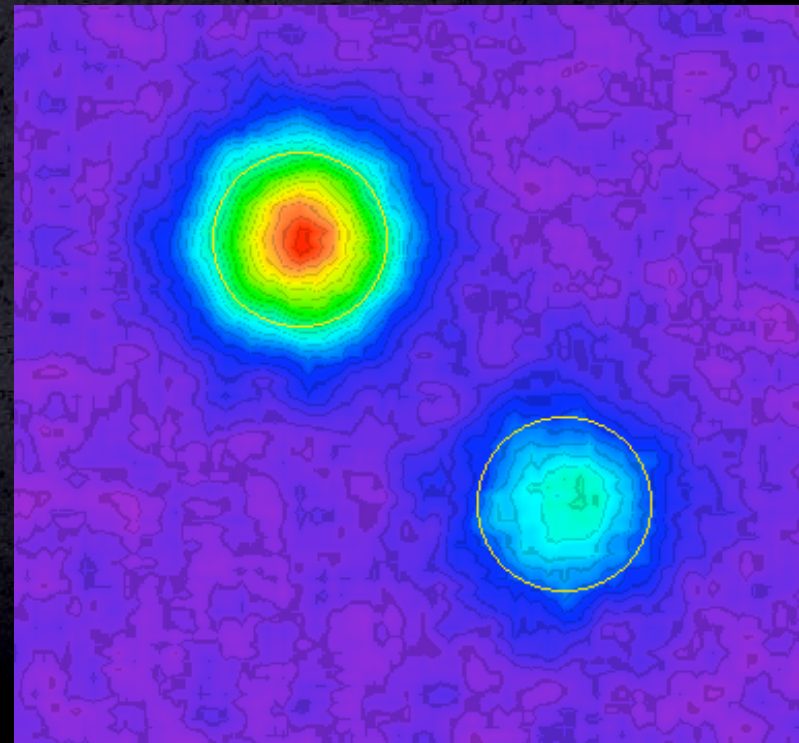
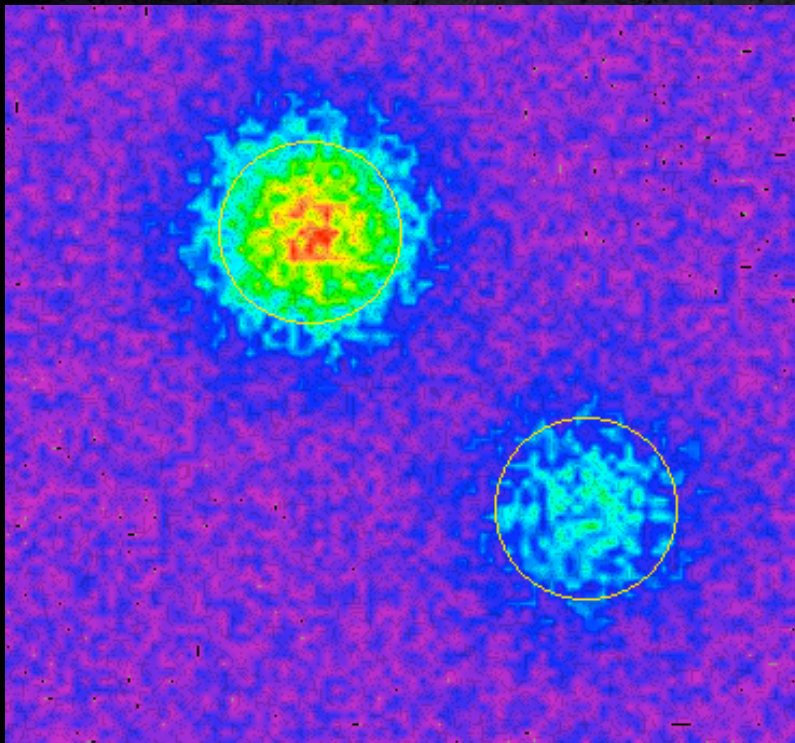
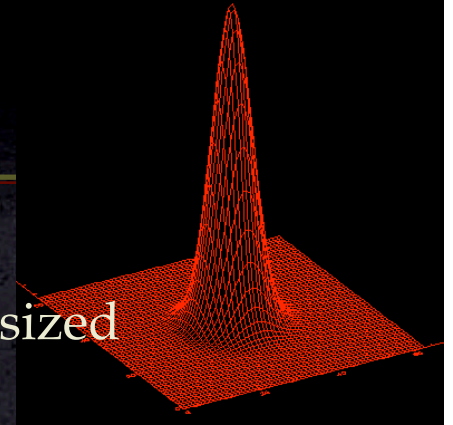
# Smoothing - spatial

● Increase S:N

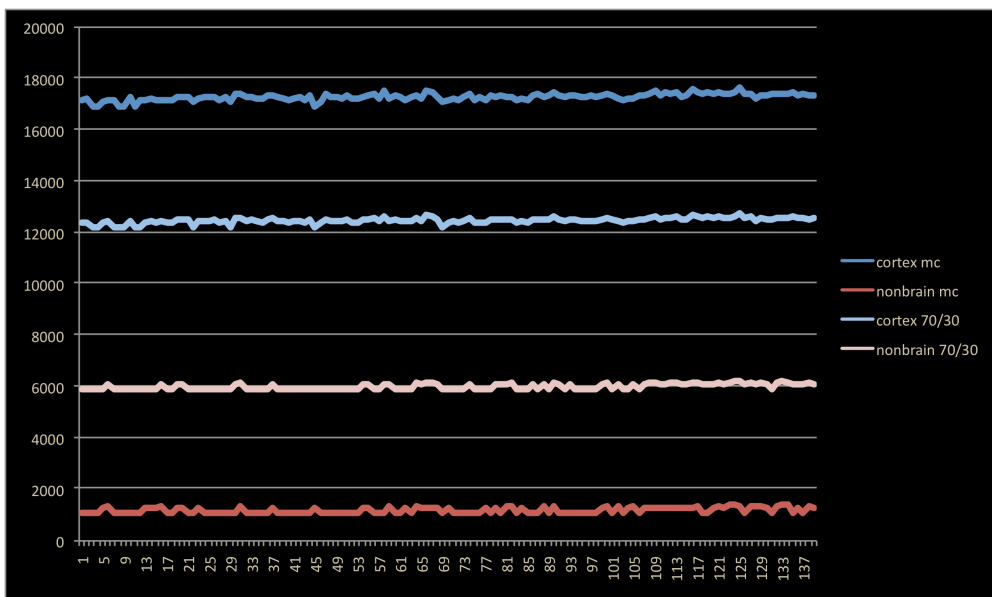
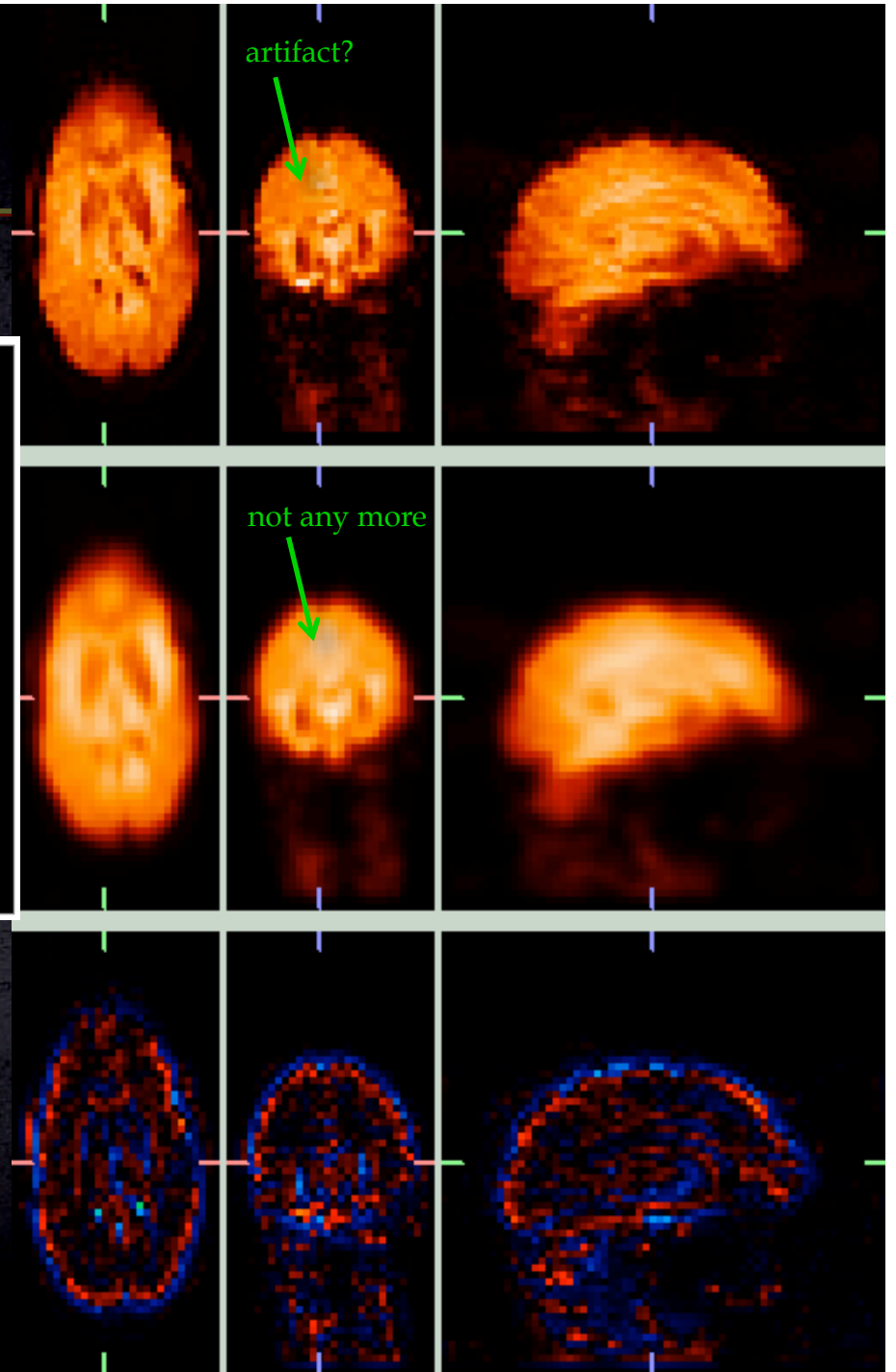
- Objects similar in size to smoothing kernel emphasized
- matched filter theorem

● Manage imperfect registration

● Fulfill "Gaussian random field" assumption



# Smoothing





# Smoothing – when?

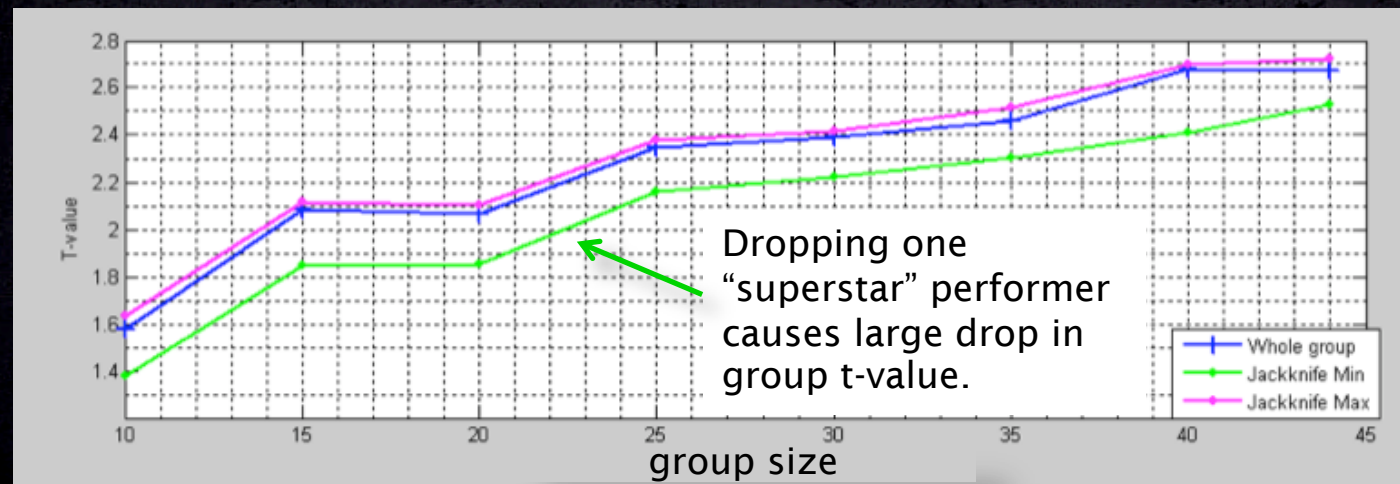
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- EPI time series
  - Spatial smoothing removes small (uninteresting) clusters
  - Mild temporal smoothing beneficial:
    - trend removal
    - high-pass filter
    - most versatile if left until GLM stage
- Parameter estimate (cluster) maps
  - more versatile for analysis
  - changes fitted results



# Group-wise artifacts

- Multi-subject or 2nd-level analysis
- subject-to-subject variance dominates
- most analysis assume:
  - similar within-subject variance
  - similar data acquisition, analysis



# Software Recommendations

## ● fMRI - specific

- AFNI, FSL, SPM have largest market share, similar results
- Two- step procedure for selecting software:
  - Find the smartest person in your lab.
  - Use what they use.

## ● Scripting

- bash
  - fast, easy, universal
  - idiosyncratic, hard to distribute
- Python
  - versatile, extensible, good for distribution
  - mostly universal, moderate learning curve
- Matlab, IDL
- sed & awk? You don't need my advice.

## ● Other handy tools:

- R <http://www.r-project.org/>
- fmristat <http://www.math.mcgill.ca/keith/fmristat/>
- NiPy <http://neuroimaging.scipy.org/>