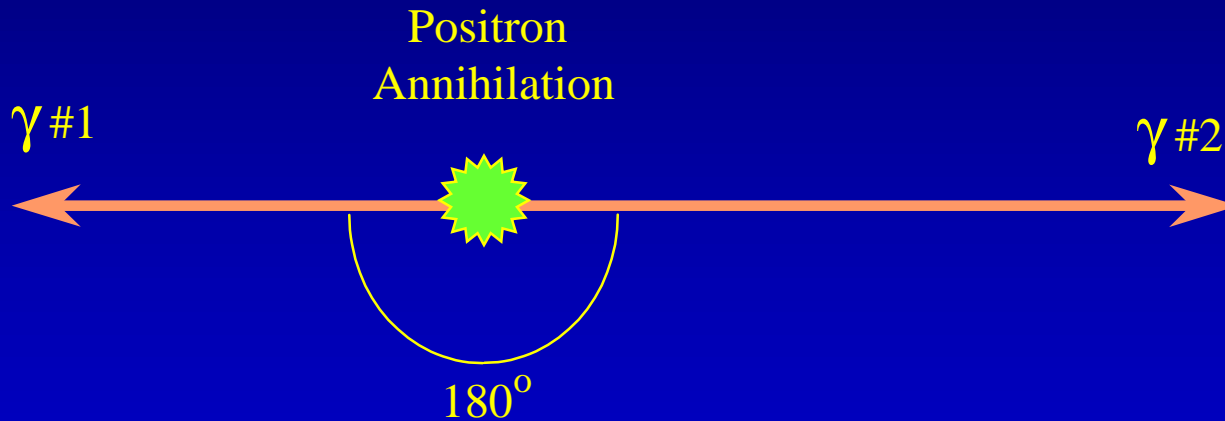
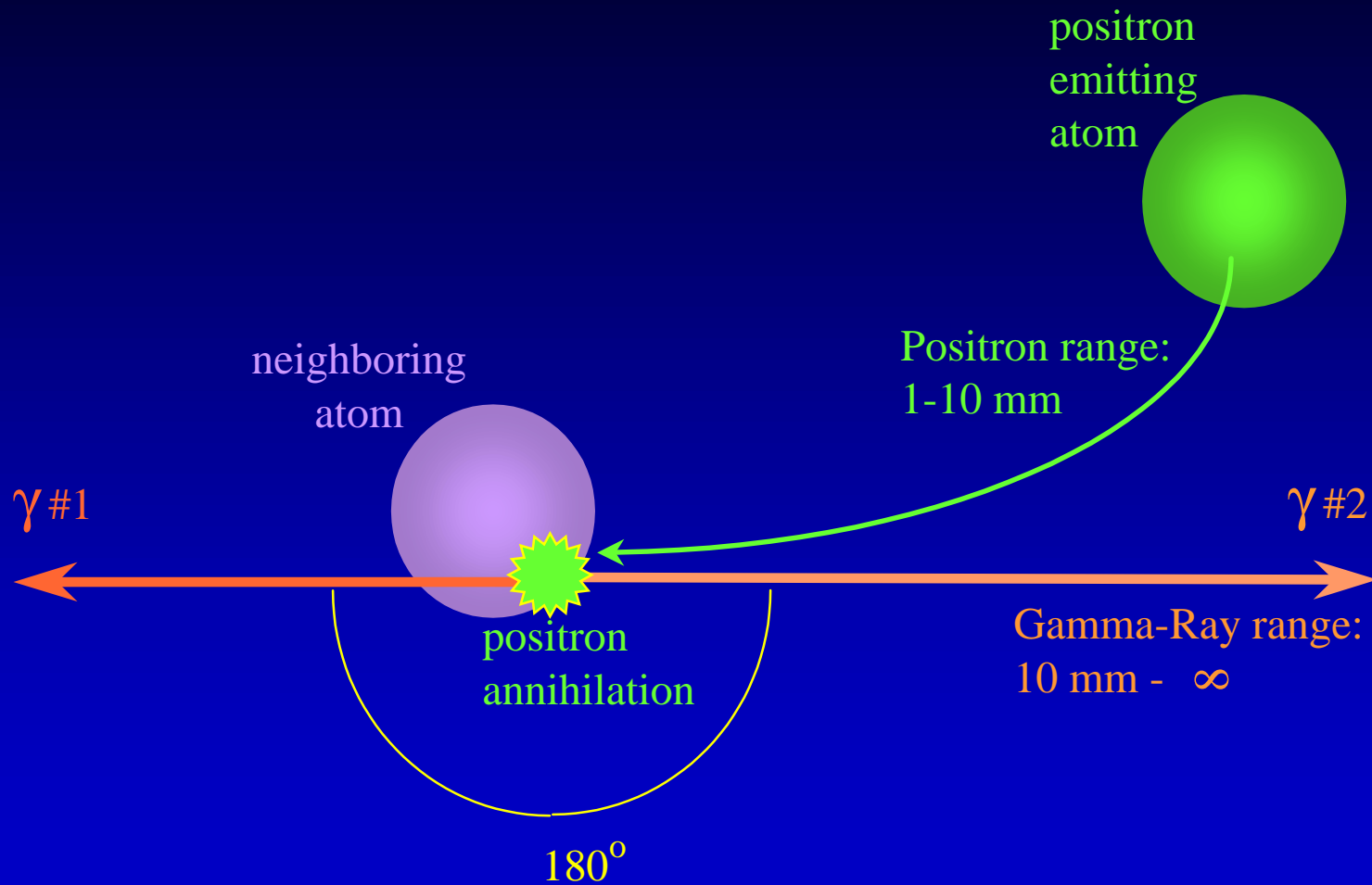


Introduction to Positron Emission Tomography

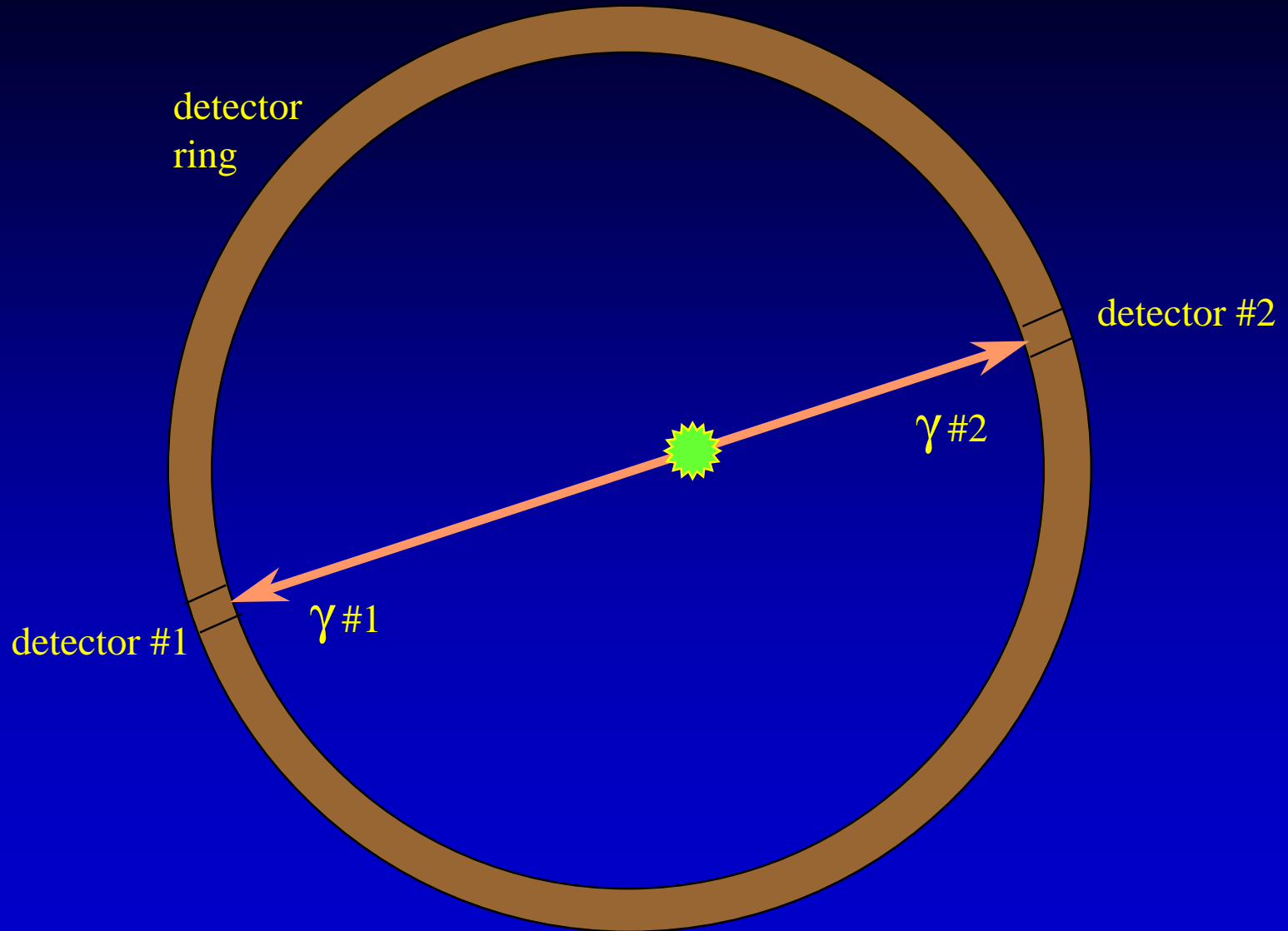
with your host, Terry Oakes



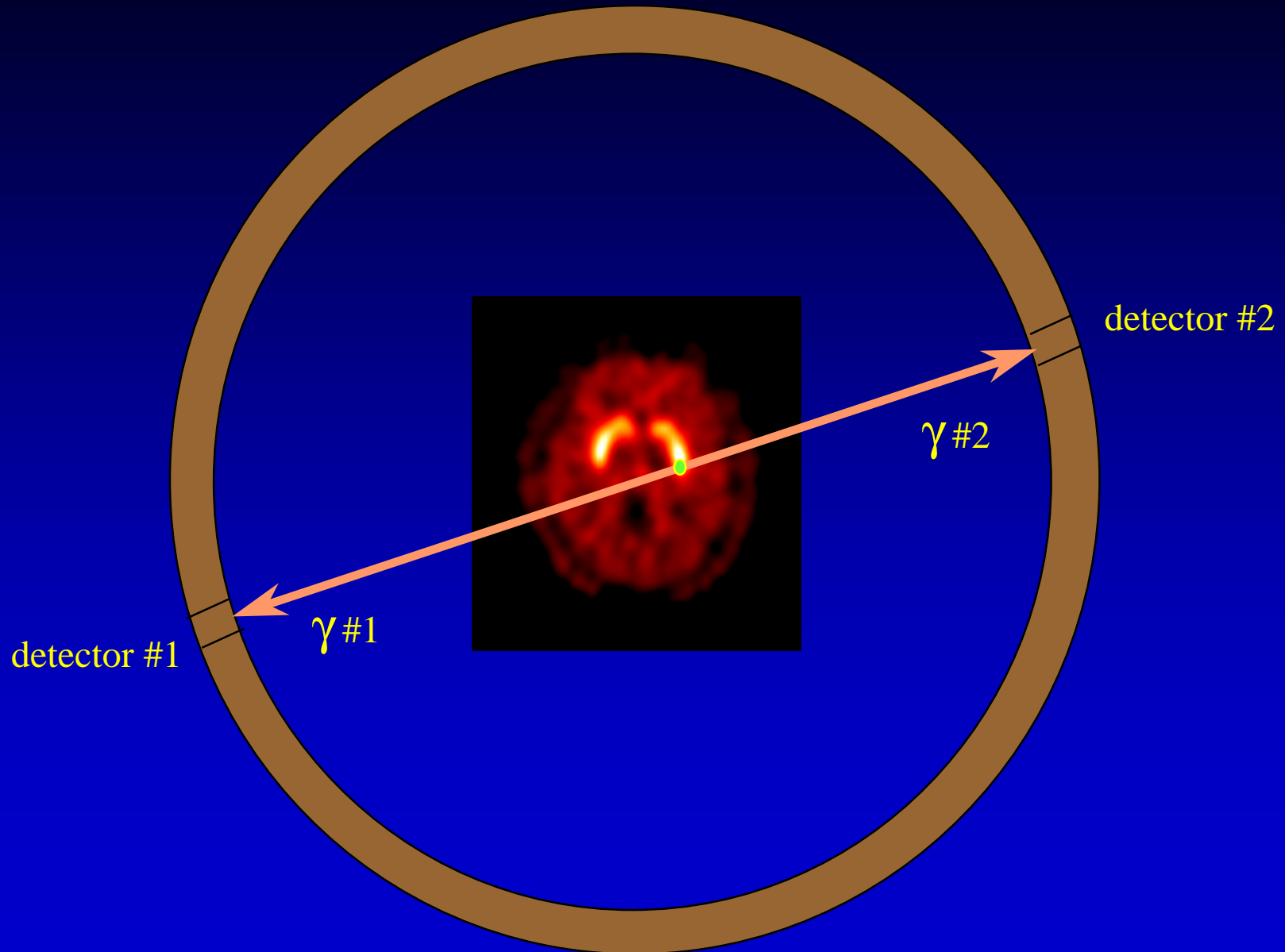
Positron Annihilation



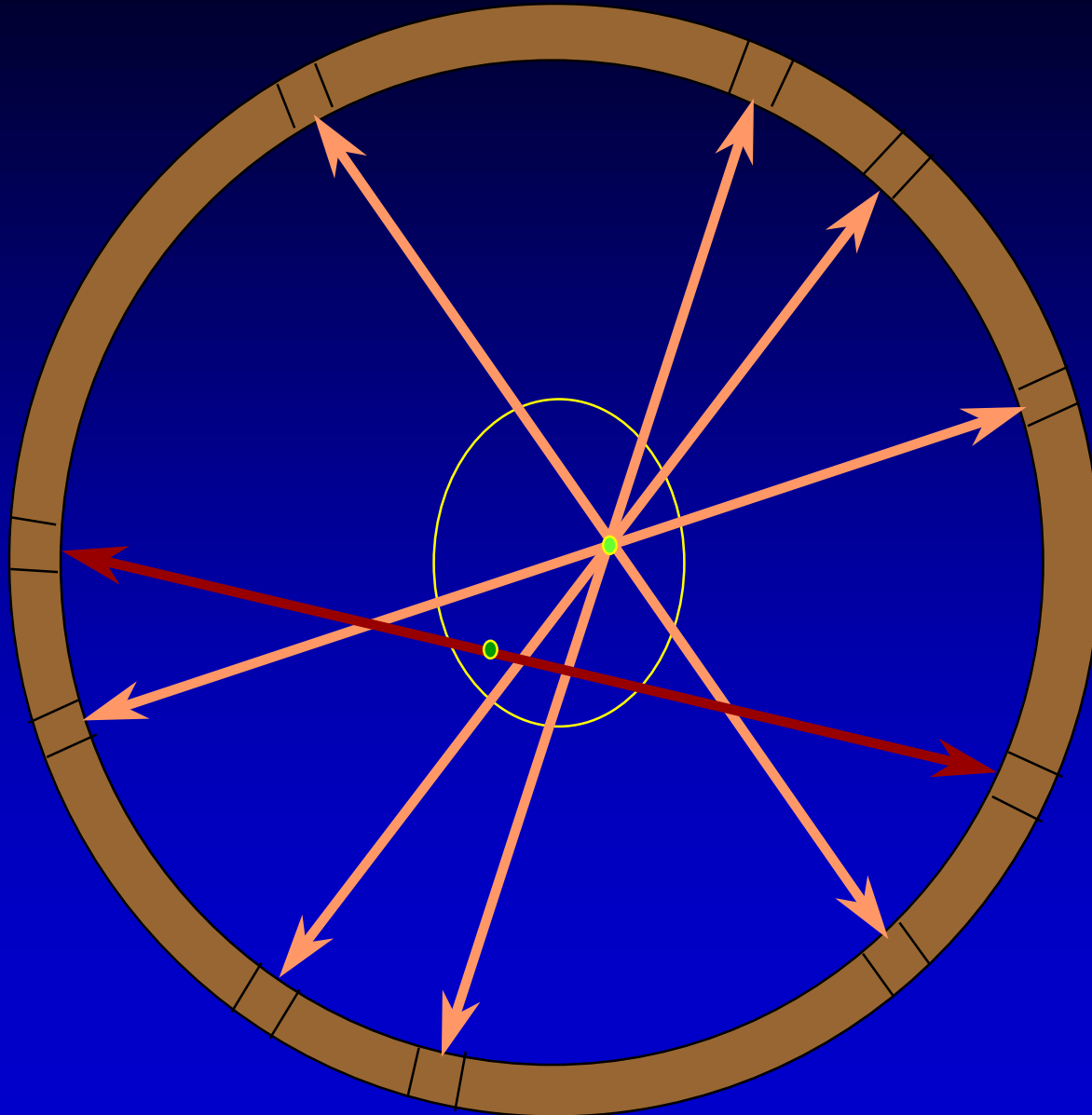
Positron Emission Tomography



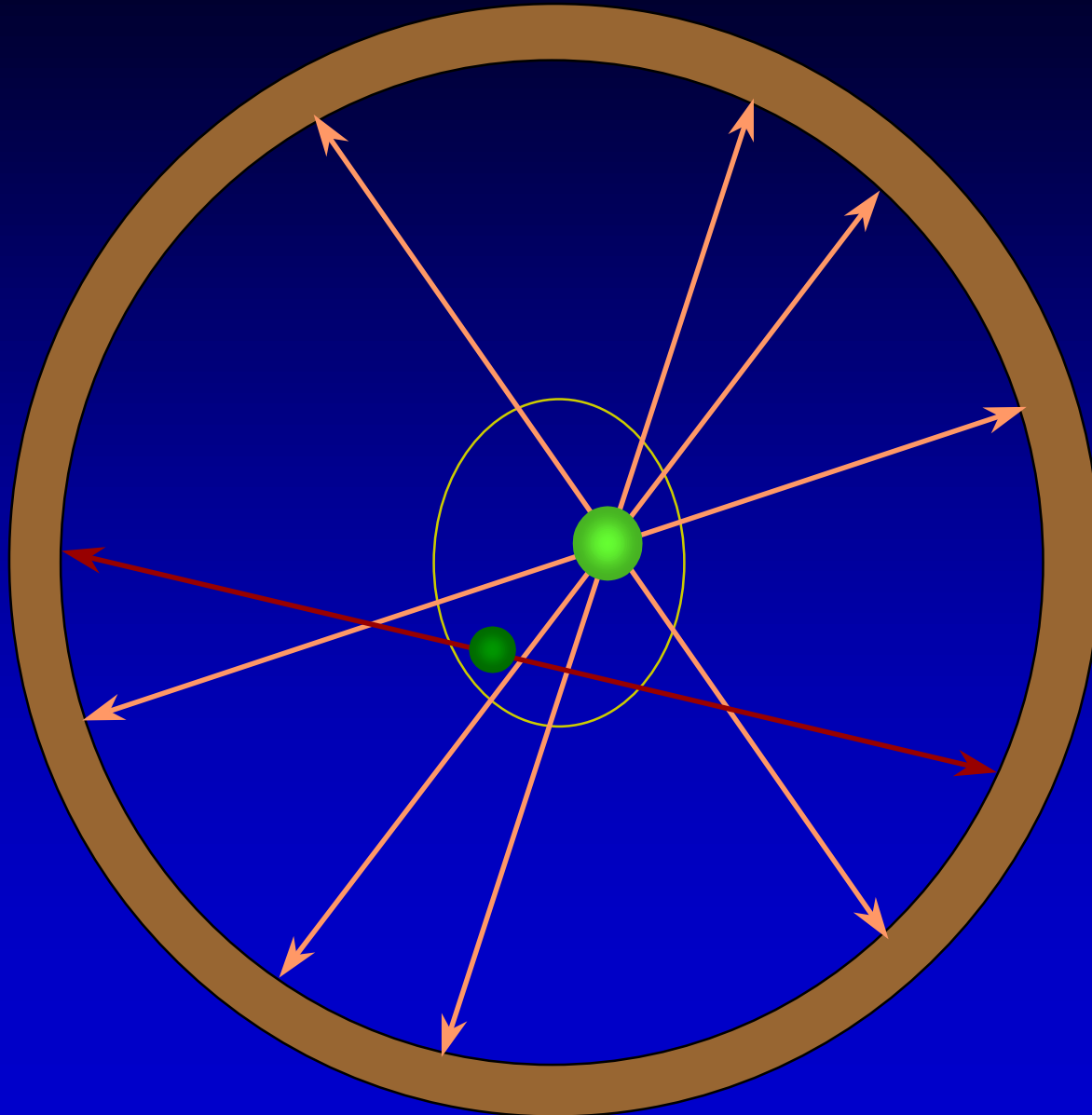
Positron Emission Tomography



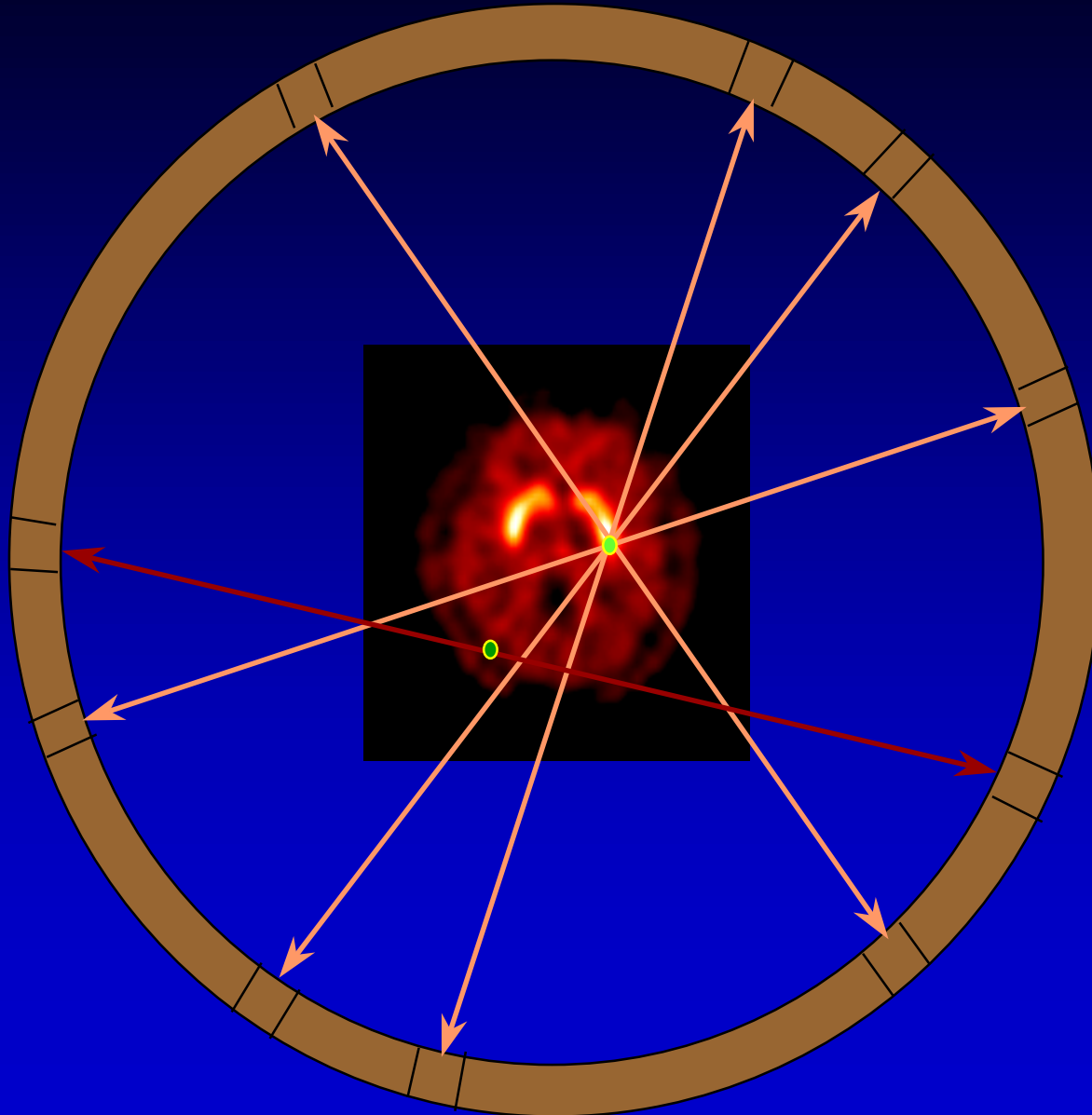
Positron Emission Tomography



Positron Emission Tomography



Positron Emission Tomography

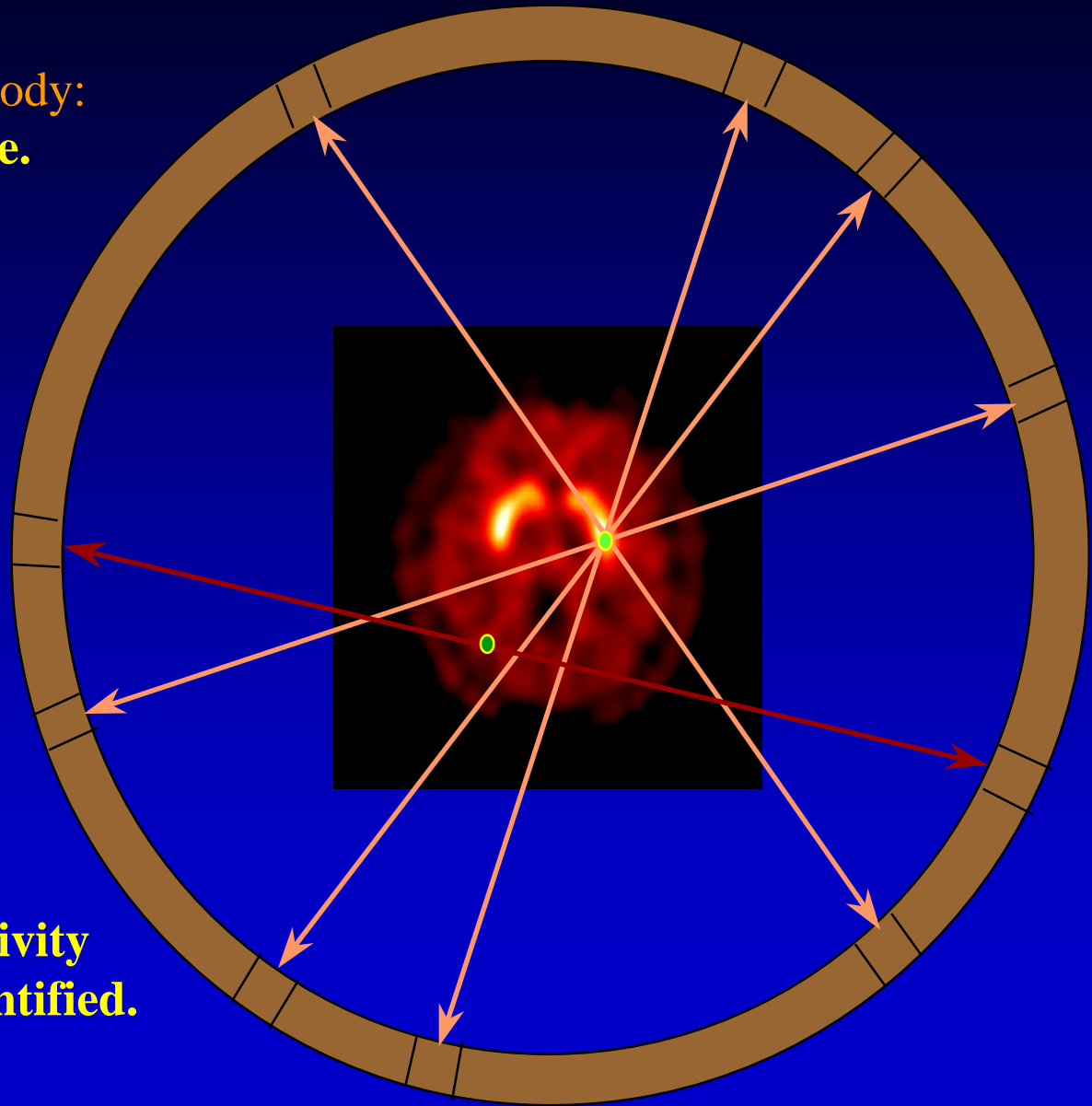


P.E.T. measures Concentration of Radioactivity

1) Gamma-rays escape from body:
External detection possible.

2) Two gamma rays emitted
at 180° when a positron
annihilates:
**The annihilation occurred
somewhere between
the two detectors.**

3) Regions with greater
radioactivity levels
produce more LORs:
**Concentration of radioactivity
can be measured and quantified.**

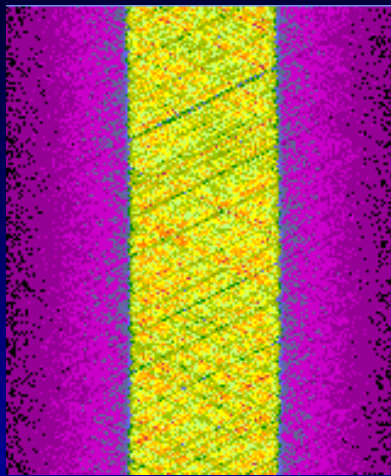


**P.E.T. yields Quantitative results.
($\mu\text{Ci/cc}$ tissue)**

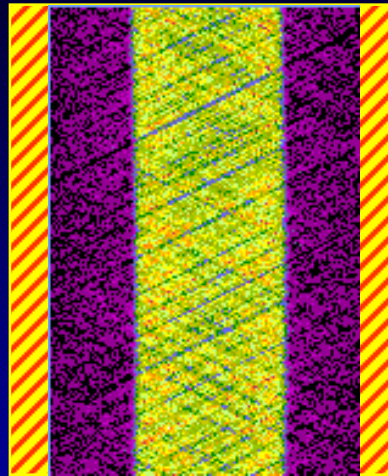
Corrections must be applied to raw data:

- 1) Dead-time, Random events**
- 2) Calibration**
- 3) Normalization**
- 4) Scatter-correction**
- 5) Attenuation correction**
- 6) Reconstruction**

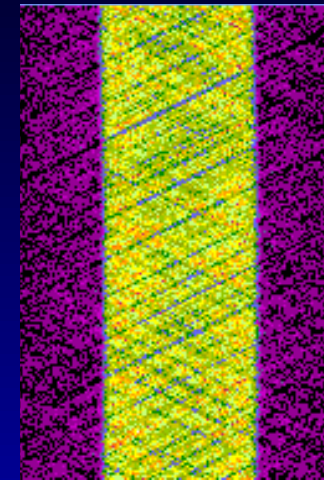
Corrections to Sinograms



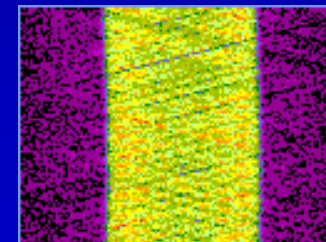
raw sinogram
(20 cm cylinder)



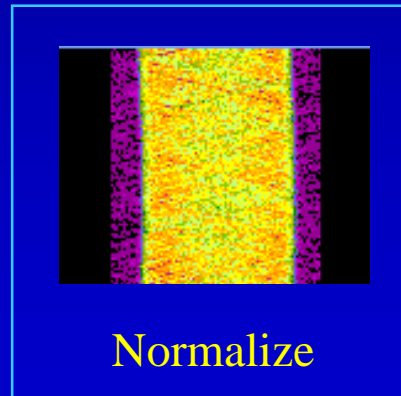
trim
(remove edges)



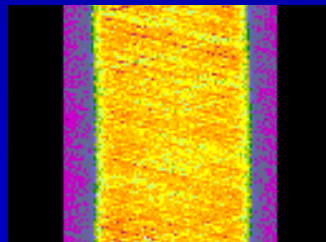
Scatter-Correct



mash
(combine angular views)



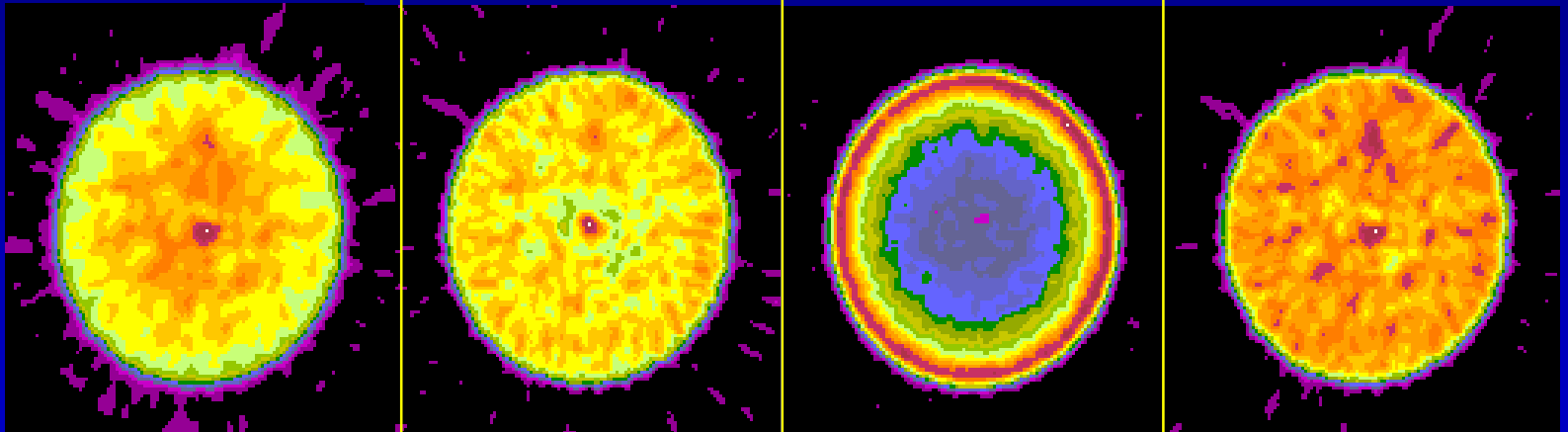
Normalize



Normalized,
without Scatter-Correction

Effect of Corrections on Images

Scatter-corrected		X	X	X
Normalized	X		X	X
Attenuation-corrected	X	X		X



Uniform
20 cm cylinder



color scale

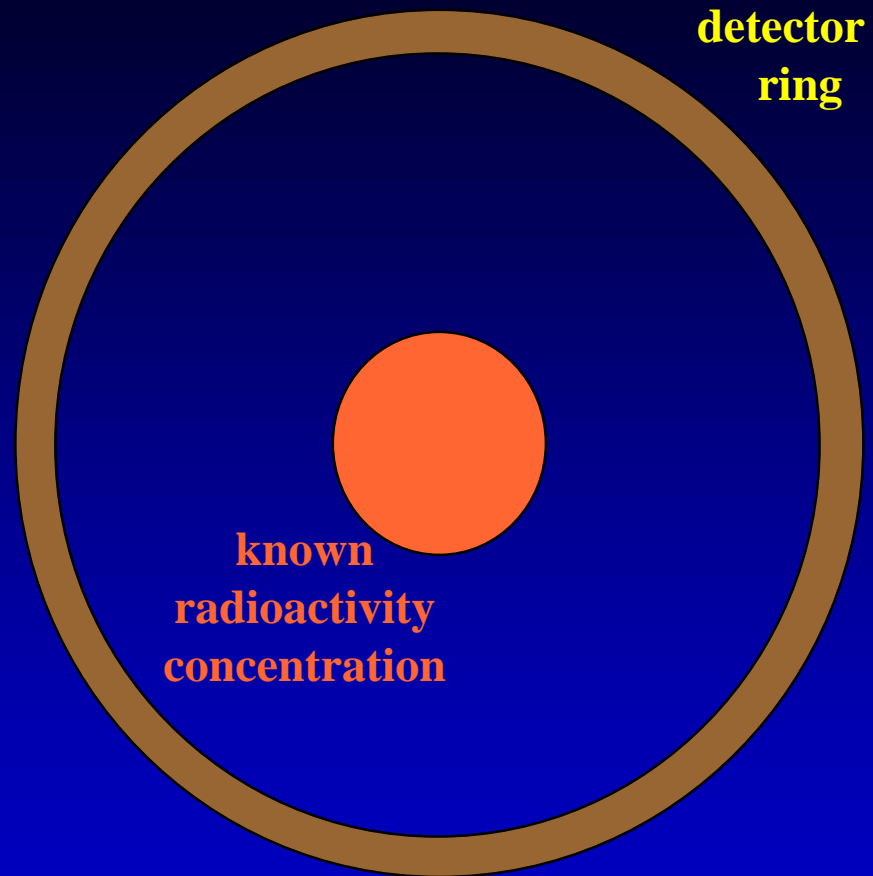
Calibration

Converting
“counts/pixel”
to
“microCi / cc tissue”

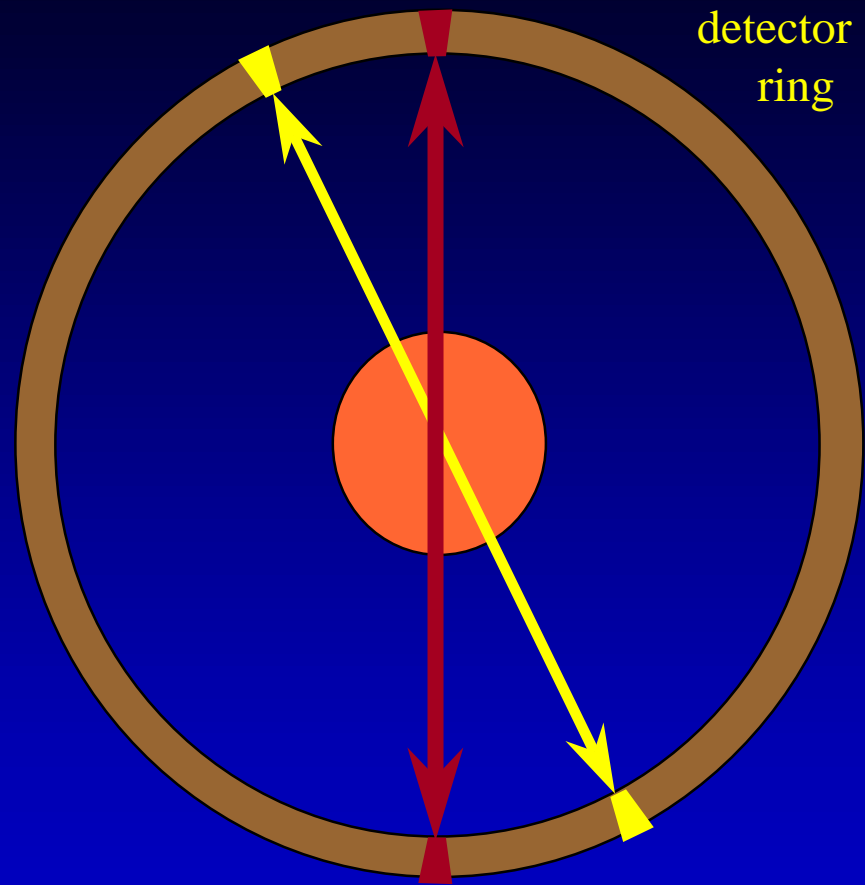
Measure response of
the PET scanner to a
known concentration
of radioactivity.



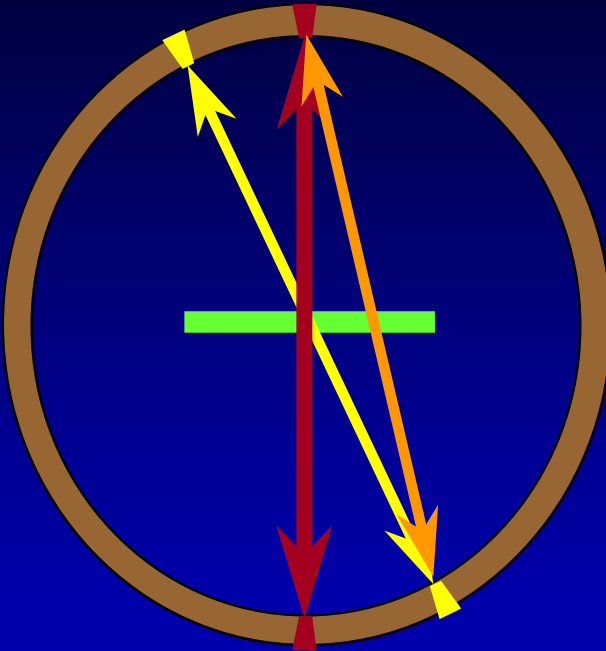
Obtain
Calibration Factor
applicable for all scans.
($CF \sim (\mu\text{Ci/cc})/\text{counts}$)



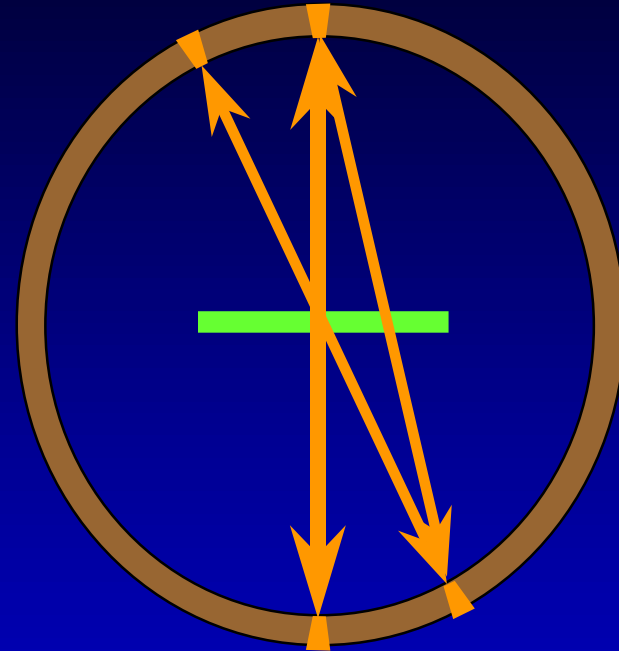
Normalization



Normalization



Individual detectors respond differently to the same level of radioactivity.



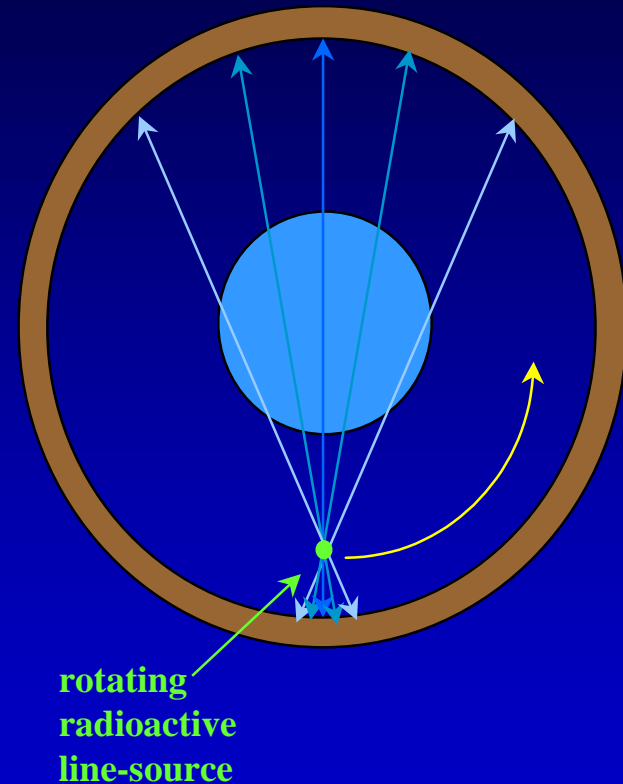
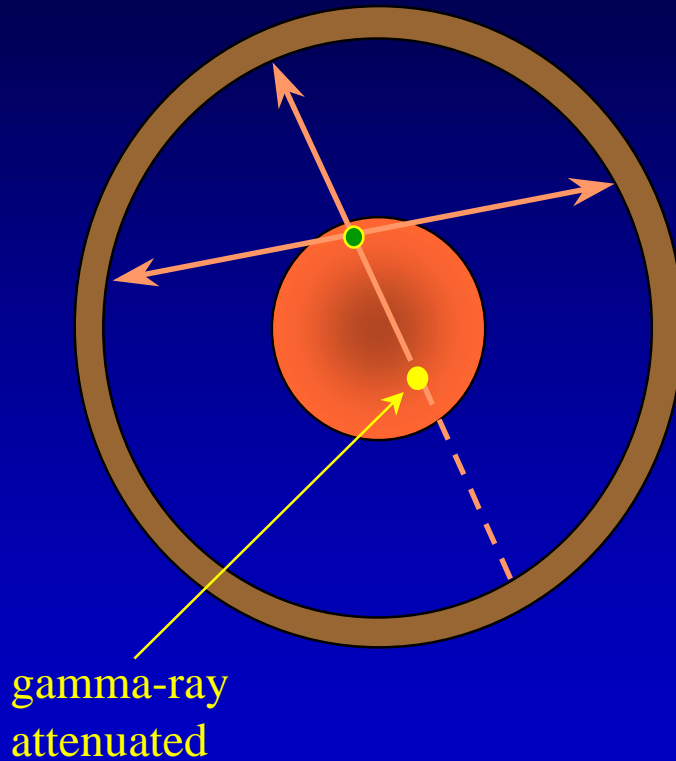
Normalization produces a uniform response to the same level of radioactivity.

Attenuation Correction

Gamma-ray attenuation proportional to:

- 1) density of object
- 2) pathlength through object

Attenuation can be corrected with a density-weighted map of the object.

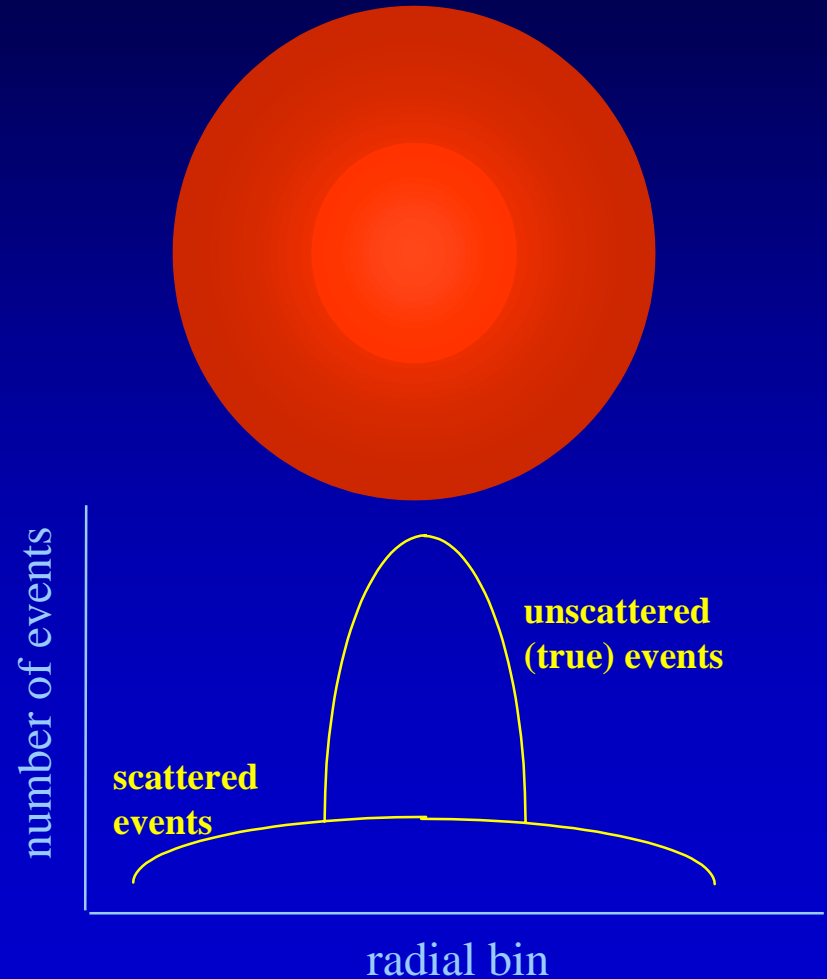
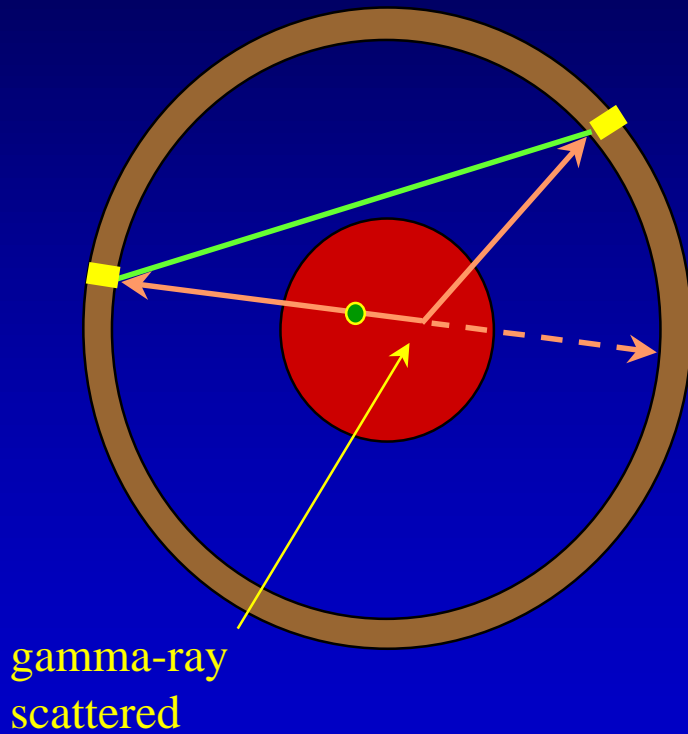


**Attenuation causes a non-uniform loss of events;
more gamma rays passing through the middle of the object are lost.**

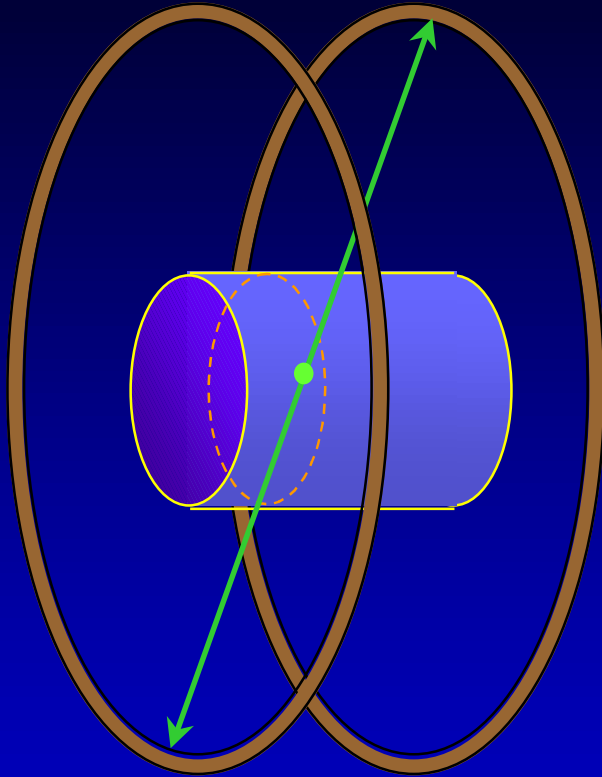
Scatter Correction

Scattered gamma rays cause recorded events to be mispositioned.

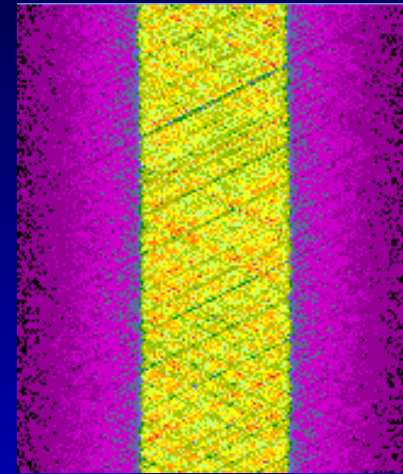
Scatter tends to increase the concentration measured toward the center of the object.



PET Data Acquisition

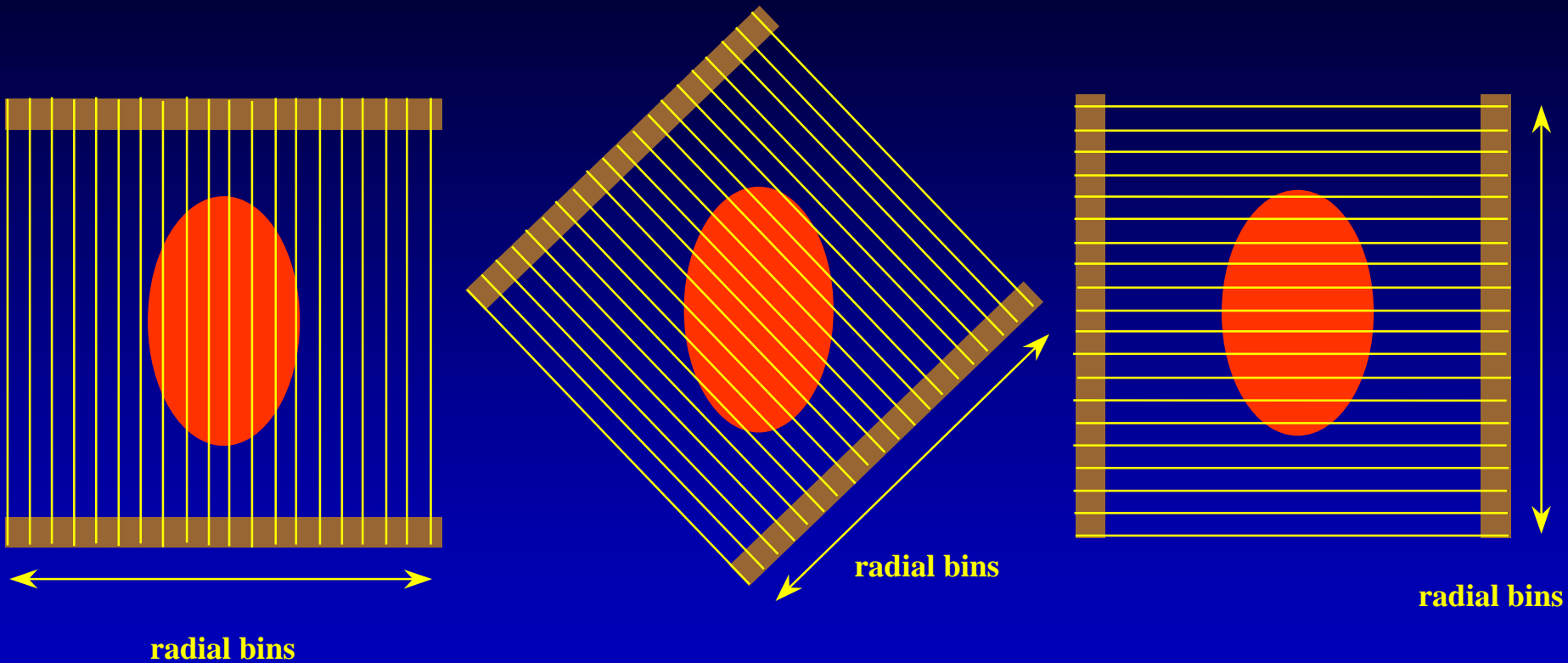


Radioactive source
in PET scanner



raw sinogram

P.E.T. data are acquired as discrete Lines of Response (LORs)

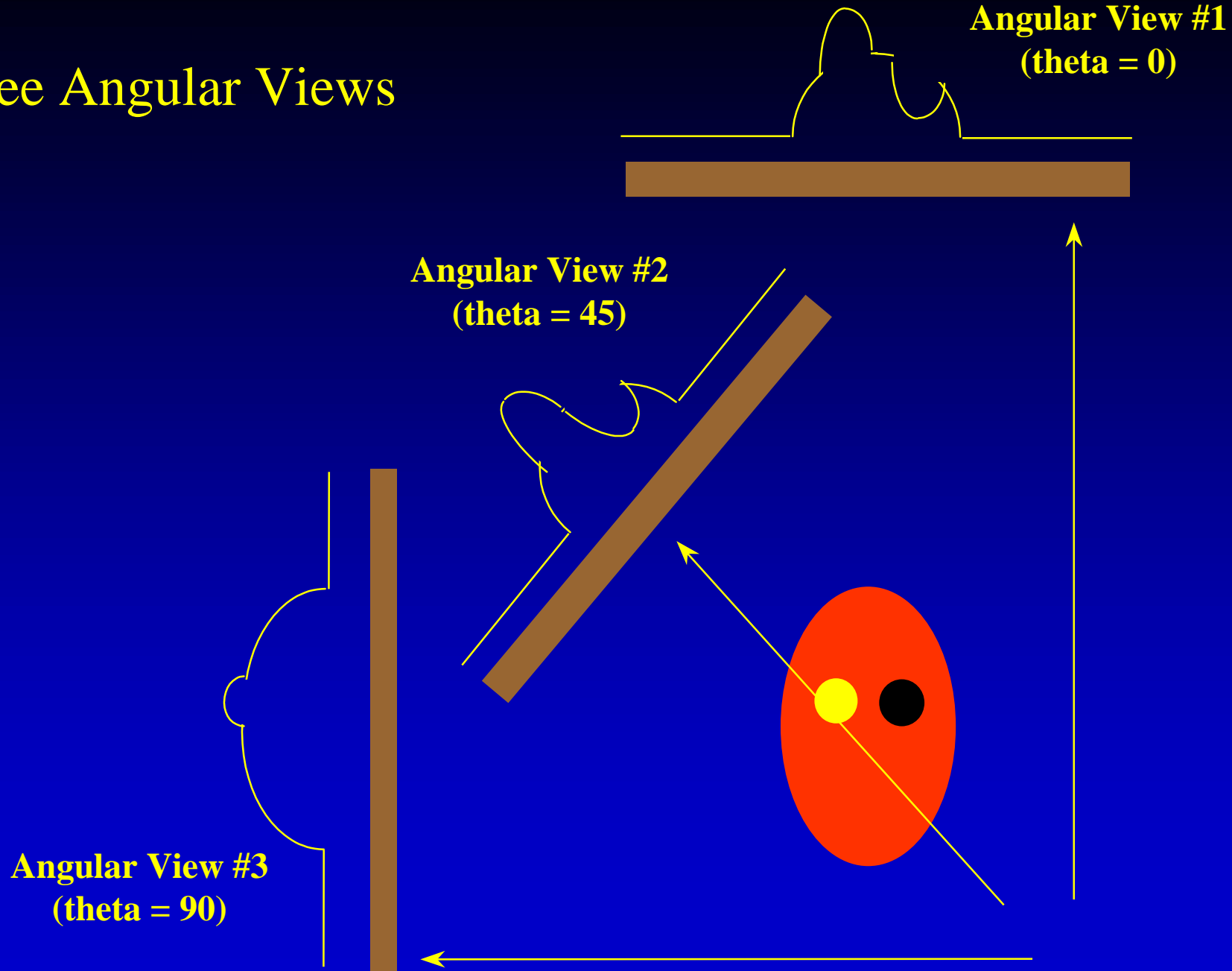


Angular View #1
(theta = 0)

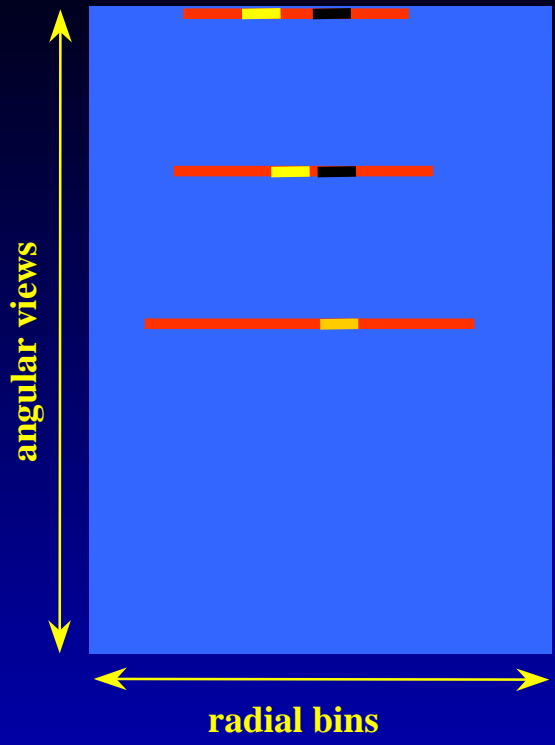
Angular View #2
(theta = 45)

Angular View #3
(theta = 90)

Three Angular Views



Sinogram

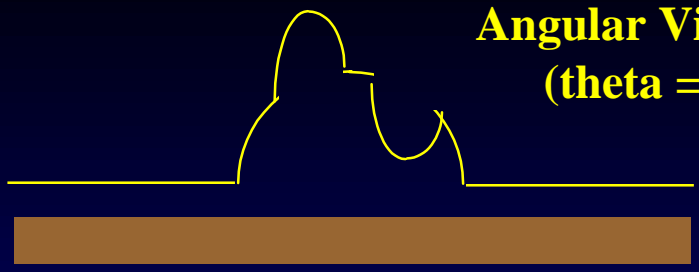


#1

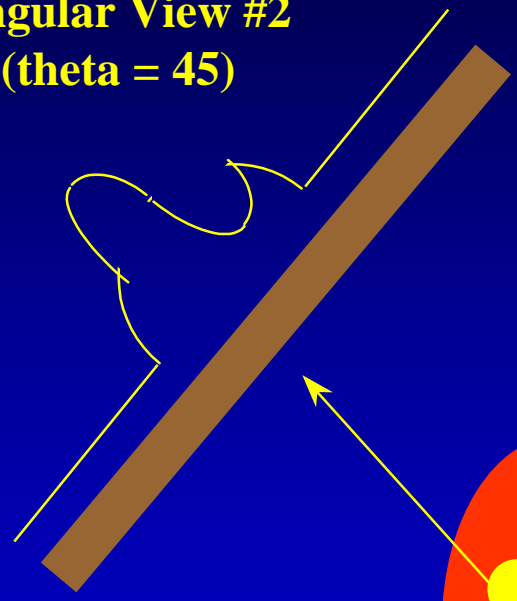
#2

#3

Angular View #1
(theta = 0)



Angular View #2
(theta = 45)



Angular View #3
(theta = 90)

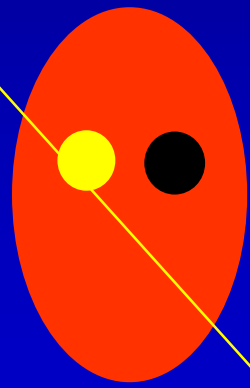
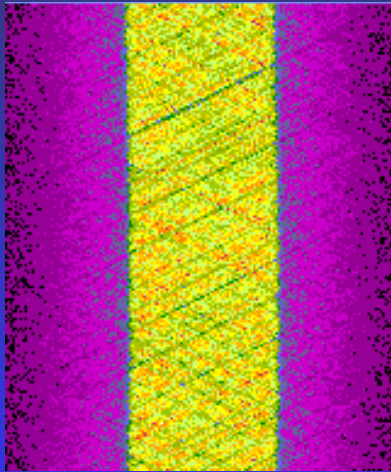
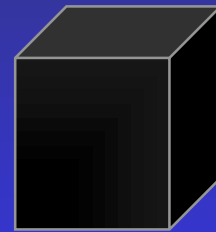


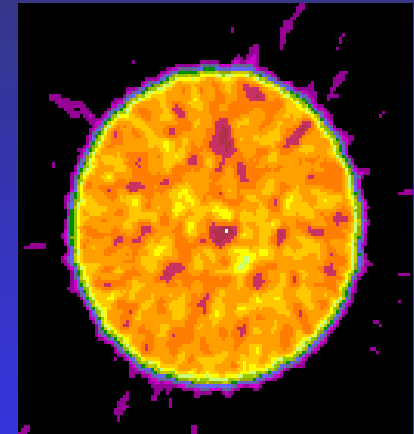
Image Reconstruction



raw sinogram



it's magic!



Reconstructed Image